

DECLARATION

I, Masayuki Sakai, c/o Fukami Patent Office, Nakanoshima Central Tower,  
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declare:

that I know well both the Japanese and English languages;

that to the best of my knowledge and belief the English translation  
attached hereto is a true and correct translation of Japanese Patent Application  
No. 2001-400519, filed on December 28, 2001;

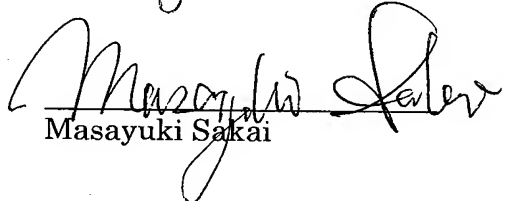
that all statements made of my own knowledge are true;

that all statements made on information and belief are believed to be true;

and

that the statements are made with the knowledge that willful false  
statements and the like are punishable by fine or imprisonment, or both, under 18  
USC 1001.

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[Document Name] Specification

[Title of the Invention] Brain Current Source Estimating Method, Brain Current Source Estimating Program, and Brain Current Source Estimating Apparatus

[Scope of Claims for Patent]

[Claim 1] A brain current source estimating method for estimating, based on an electromagnetic field observed outside a scalp, a position of a current source as a source of said electromagnetic field existing in the brain, comprising the steps of:

setting, in the brain, a plurality of virtual curved surfaces having depths from brain surface different from each other and shapes not intersecting with each other, and setting lattice points on each of said virtual curved surfaces;

estimating, on each of said virtual curved surfaces, a current distribution for recovering said observed electromagnetic field; and

based on an expansion of the current distribution estimated on said virtual curved surfaces and a difference between the electromagnetic field recovered based on said current distribution and said observed electromagnetic field, identifying a virtual curved surface at which said expansion and said difference attain relative minimums among said plurality of virtual curved surfaces as a true curved surface on which said current source exists.

[Claim 2] The brain current source estimating method according to claim 1, wherein

said step of estimating a current distribution includes the step of

determining posterior probability by Bayesian estimation method from prior distribution and observation data of said electromagnetic field, and

said step of identifying as a true curved surface on which said current source exists includes the step of

identifying a virtual curved surface of which corresponding said posterior probability attains the maximum, among said virtual curved surfaces.

[Claim 3] The brain current source estimating method according to claim 2,

wherein

said step of estimating a current distribution includes the step of

identifying a first virtual curved surface closest to said brain surface and having posterior probability attaining a relative maximum, among said plurality of virtual curved surfaces, while successively moving from a virtual curved surface on the side of the brain surface to a deeper side, and

said step of identifying a curved surface as a true curved surface on which said current source exists includes the steps of

identifying a localized current distribution corresponding to a point of relative maximum of said current distribution, on said first virtual curved surface,

separating a plurality of local surfaces each including said localized current distribution, and

fixing, among said plurality of local surfaces, local surfaces other than a local surface as an object of identification, moving said local surface as an object of identification in the depth direction, and identifying positions where said posterior probability attains the relative maximum, successively from the side closer to said brain surface.

[Claim 4] The brain current source estimating method according to claim 3, wherein

in said step of estimating a current distribution, said current distribution is estimated with a first spatial resolution,

said method further comprising the step of

re-estimating said current distribution with a second spatial resolution higher than said first spatial resolution and resolution of said plurality of virtual curved surfaces in the depth direction being improved.

[Claim 5] A program for a computer for estimating, based on an electromagnetic field observed outside a scalp, a position of a current source as a source of said electromagnetic field existing in the brain, to have the computer execute the

steps of:

setting, in the brain, a plurality of virtual curved surfaces having depths from brain surface different from each other and shapes not intersecting with each other, and setting lattice points on each of said virtual curved surfaces;

estimating, on each of said virtual curved surfaces, a current distribution for recovering said observed electromagnetic field; and

based on an expansion of the current distribution estimated on said virtual curved surfaces and a difference between the electromagnetic field recovered based on said current distribution and said observed electromagnetic field, identifying a virtual curved surface at which said expansion and said difference attain relative minimums among said plurality of virtual curved surfaces as a true curved surface on which said current source exists.

[Claim 6] The program according to claim 5, wherein  
 said step of estimating a current distribution includes the step of  
 determining posterior probability by Bayesian estimation method from prior distribution and observation data of said electromagnetic field, and  
 said step of identifying as a true curved surface on which said current source exists includes the step of  
 identifying a virtual curved surface of which corresponding said posterior probability attains the maximum, among said virtual curved surfaces.

[Claim 7] The program according to claim 6, wherein  
 said step of estimating a current distribution includes the step of  
 identifying a first virtual curved surface closest to said brain surface and having posterior probability attaining a relative maximum, among said plurality of virtual curved surfaces, while successively moving from a virtual curved surface on the side of the brain surface to a deeper side, and  
 said step of identifying a curved surface as a true curved surface on which said current source exists includes the steps of

identifying a localized current distribution corresponding to a point of relative maximum of said current distribution, on said first virtual curved surface,

separating a plurality of local surfaces each including said localized current distribution, and

fixing, among said plurality of local surfaces, local surfaces other than a local surface as an object of identification, moving said local surface as an object of identification in the depth direction, and identifying positions where said posterior probability attains the relative maximum, successively from the side closer to said brain surface.

[Claim 8] The program according to claim 7, wherein  
in said step of estimating a current distribution, said current distribution is estimated with a first spatial resolution,

said program further comprising the step of  
re-estimating said current distribution with a second spatial resolution higher than said first spatial resolution and resolution of said plurality of virtual curved surfaces in the depth direction being improved.

[Claim 9] A brain current source estimating apparatus for estimating, based on an electromagnetic field observed outside a scalp, a position of a current source as a source of said electromagnetic field existing in the brain, comprising:

virtual curved surface setting means for setting, in the brain, a plurality of virtual curved surfaces having depths from brain surface different from each other and shapes not intersecting with each other, and setting lattice points on each of said virtual curved surfaces;

current distribution estimating means for estimating, on each of said virtual curved surfaces, a current distribution for recovering said observed electromagnetic field; and

current source identifying means for identifying, based on an expansion of the current distribution estimated on said virtual curved surfaces and a difference between

the electromagnetic field recovered based on said current distribution and said observed electromagnetic field, a virtual curved surface at which said expansion and said difference attain relative minimums among said plurality of virtual curved surfaces as a true curved surface on which said current source exists.

[Claim 10] The brain current source estimating apparatus according to claim 9, wherein

said current distribution estimating means includes

posterior probability determining means for determining posterior probability by Bayesian estimation method from prior distribution and observation data of said electromagnetic field, and

said current source identifying means includes

virtual curved surface identifying means for identifying a virtual curved surface of which corresponding said posterior probability attains the maximum, among said virtual curved surfaces.

[Claim 11] The brain current source estimating apparatus according to claim 10, wherein

said current distribution estimating means includes

shallowest virtual curved surface identifying means for identifying a first virtual curved surface closest to said brain surface and having posterior probability attaining a relative maximum, among said plurality of virtual curved surfaces, while successively moving from a virtual curved surface on the side of the brain surface to a deeper side, and

said current source identifying means includes

localized current distribution identifying means for identifying a localized current distribution corresponding to a point of relative maximum of said current distribution, on said first virtual curved surface,

local surface extracting means for separating a plurality of local surfaces each including said localized current distribution, and



local surface position identifying means for fixing, among said plurality of local surfaces, local surfaces other than a local surface serving as an object of identification, moving said local surface as an object of identification in the depth direction, and identifying positions where said posterior probability attains the relative maximum, successively from the side closer to said brain surface.

[Claim 12] The brain current source estimating apparatus according to claim 11, wherein

said current distribution estimating means initially estimates said current distribution with a first spatial resolution and thereafter re-estimates said current distribution with a second spatial resolution higher than said first spatial resolution and resolution of said plurality of virtual curved surfaces in the depth direction being improved.

#### [Detailed Description of the Invention]

##### [Technical Field to Which the Invention Belongs]

The present invention relates to a method of estimating position or distribution of a brain current source or sources generating magnetic fields or electric fields outside a scalp in correspondence with brain activities, as well as to a brain current source estimating program and to a brain current source estimating apparatus.

##### [Prior Art]

Thanks to remarkable development in the field of biomedical measurement technique, precision in measuring weak electric field (brain wave) or weak magnetic field (brain magnetic wave) generated from the brain, of which measurement has been difficult and error-prone, has been improved year by year.

Specifically, receiving external stimuli, neural cells in the brain generate a current. The current results in the aforementioned weak electric field or weak magnetic field. Here, "brain wave" refers to the electric field generated from the brain by the current from the neural cells. An "electroencephalogram: EEG" refers to a method of measuring the brain wave.

The “brain magnetic wave” refers to a magnetic field generated from the brain by the current from the neural cells. A “magnetoencephalography: MEG” refers to a method of measuring the brain magnetic wave. A crucial advantage of the magnetoencephalography is that, as the magnetic field is almost free of any influence of volume conductor, it is expected that relatively accurate three-dimensional estimation of the position of a brain current source can be attained by measuring magnetism from outside one’s scalp.

In the analysis of the brain magnetic wave, an active portion of the brain is estimated in a non-invasive manner, by measuring the generated magnetic field from outside the brain.

The magnetic field, however, is so weak that it is very susceptible to the influence of external magnetic field such as terrestrial magnetism. Therefore, the weak magnetic field is measured by a Superconducting QUantum Interference Device (SQUID), which is a measuring device utilizing superconductivity, within a shield that shuts out any external magnetic field.

[Problems to be Solved by the Invention]

It is noted, however, that in the field of studying algorithms for “estimating positions of brain current source,” decisive method is non-existent at present, though various and many variations of initial models have been tried.

By way of example, “dipole estimation method” as one algorithm for “estimating positions of brain current sources,” is disclosed in Reference 1: J. C. Mosher, P. S. Lewis and R. M. Leahy, IEEE Trans. Biomed. Engng. <1992> vol. 39, pp.541-557. In the “dipole estimation method,” however, the position of a dipole is estimated from observed magnetic field, assuming that the current source in the brain can be represented by one or a number of current dipoles, and this method is disadvantageous in that it is difficult to determine the number of dipoles.

As another algorithm, “spatial filtering method” is disclosed in Reference 2: K. Toyama, K. Yoshikawa, Y. Yoshida, Y. Kondo, S. Tomita, Y. Takanashi, Y. Ejima,

and S. Yoshizawa, Neuroscience, 1999, 91 (2), pp. 405-415. In the “spatial filtering method,” location of a brain current source is restricted in consideration of physiological findings, and distribution of dipoles is estimated. This method is disadvantageous in that accurate estimation of the depth of the current source is not possible.

The present invention was made to solve the above-described problems, and an object of the present invention is to provide a brain current source estimating method that enables estimation of a position, depth direction inclusive, of a brain current source from observed data.

Another object of the present invention is to provide a brain current source estimating method that enables estimation of positions of a plurality of brain current sources from observed data, even when there are a plurality of brain current sources.

A still further object of the present invention is to provide a brain current source estimating program that enables estimation of a position, depth direction inclusive, of a brain current source from observed data.

A still further object of the present invention is to provide a brain current source estimating program that enables estimation of positions of a plurality of brain current sources from observed data, even when there are a plurality of brain current sources.

A still further object of the present invention is to provide a brain current source estimating apparatus that enables estimation of a position, depth direction inclusive, of a brain current source from observed data.

A still further object of the present invention is to provide a brain current source estimating apparatus that enables estimation of positions of a plurality of brain current sources from observed data, even when there are a plurality of brain current sources.

#### [Means for Solving the Problems]

In order to attain such objects, a brain current source estimating method according to the present invention is a method for estimating, based on an electromagnetic field observed outside a scalp, a position of a current source as a source

of the electromagnetic field existing in the brain, including the steps of: setting, in the brain, a plurality of virtual curved surfaces having depths from brain surface different from each other and shapes not intersecting with each other and setting lattice points on each of the virtual curved surfaces; estimating, on each of the virtual curved surfaces, a current distribution for recovering the observed electromagnetic field; and based on an expansion of the current distribution estimated on the virtual curved surfaces and a difference between the electromagnetic field recovered based on the current distribution and the observed electromagnetic field, identifying a virtual curved surface at which the expansion and the difference attain relative minimums among the plurality of virtual curved surfaces as a true curved surface on which the current source exists.

Preferably, the step of estimating a current distribution includes the step of determining posterior probability by Bayesian estimation method from prior distribution and observation data of the electromagnetic field, and the step of identifying as a true curved surface on which the current source exists includes the step of identifying a virtual curved surface of which corresponding posterior probability attains the highest, among the virtual curved surfaces.

Preferably, the step of estimating a current distribution includes the step of identifying a first virtual curved surface closest to the brain surface and having posterior probability attaining a relative maximum, among the plurality of virtual curved surfaces, while successively moving from a virtual curved surface on the side of the brain surface to a deeper side, and the step of identifying a curved surface as a true curved surface on which the current source exists includes the steps of identifying a localized current distribution corresponding to a point of relative maximum of the current distribution, on the first virtual curved surface, separating a plurality of local surfaces each including the localized current distribution, and fixing, among the plurality of local surfaces, local surfaces other than a local surface as an object of identification, moving the local surface as an object of identification in the depth direction, and identifying positions where the posterior probability attains the relative maximum, successively from the side

closer to the brain surface.

Preferably, in the step of estimating a current distribution, the current distribution is estimated with a first spatial resolution, and the method further includes the step of re-estimating the current distribution with a second spatial resolution higher than the first spatial resolution and resolution of the plurality of virtual curved surfaces in the depth direction being improved.

According to another aspect of the present invention, a program for a computer for estimating, based on an electromagnetic field observed outside a scalp, a position of a current source as a source of the electromagnetic field existing in the brain, has the computer execute the steps of: setting, in the brain, a plurality of virtual curved surfaces having depths from brain surface different from each other and shapes not intersecting with each other and setting lattice points on each of the virtual curved surfaces; estimating, on each of the virtual curved surfaces, a current distribution for recovering the observed electromagnetic field; and based on an expansion of the current distribution estimated on the virtual curved surfaces and a difference between the electromagnetic field recovered based on the current distribution and the observed electromagnetic field, identifying a virtual curved surface at which the expansion and the difference attain relative minimums among the plurality of virtual curved surfaces as a true curved surface on which the current source exists.

Preferably, the step of estimating a current distribution includes the step of determining posterior probability by Bayesian estimation method from prior distribution and observation data of the electromagnetic field, and the step of identifying as a true curved surface on which the current source exists includes the step of identifying a virtual curved surface of which corresponding posterior probability attains the highest, among the virtual curved surfaces.

Preferably, the step of estimating a current distribution includes the step of identifying a first virtual curved surface closest to the brain surface and having posterior probability attaining a relative maximum, among the plurality of virtual curved surfaces,

while successively moving from a virtual curved surface on the side of the brain surface to a deeper side, and the step of identifying a curved surface as a true curved surface on which the current source exists includes the steps of identifying a localized current distribution corresponding to a point of relative maximum of the current distribution, on the first virtual curved surface, separating a plurality of local surfaces each including the localized current distribution, and fixing, among the plurality of local surfaces, local surfaces other than a local surface as an object of identification, moving the local surface as an object of identification in the depth direction, and identifying positions where the posterior probability attains the relative maximum, successively from the side closer to the brain surface.

Preferably, in the step of estimating a current distribution, the current distribution is estimated with a first spatial resolution, and the program further includes the step of re-estimating the current distribution with a second spatial resolution higher than the first spatial resolution and resolution of the plurality of virtual curved surfaces in the depth direction being improved.

According to a still further aspect of the present invention, a brain current source estimating apparatus for estimating, based on an electromagnetic field observed outside a scalp, a position of a current source as a source of the electromagnetic field existing in the brain, includes: virtual curved surface setting means for setting, in the brain, a plurality of virtual curved surfaces having depths from brain surface different from each other and shapes not intersecting with each other and setting lattice points on each of the virtual curved surfaces; current distribution estimating means for estimating, on each of the virtual curved surfaces, a current distribution for recovering the observed electromagnetic field; and current source identifying means for identifying, based on an expansion of the current distribution estimated on the virtual curved surfaces and a difference between the electromagnetic field recovered based on the current distribution and the observed electromagnetic field, a virtual curved surface at which the expansion and the difference attain relative minimums among the plurality of virtual curved

surfaces as a true curved surface on which the current source exists.

Preferably, the current distribution estimating means includes posterior probability determining means for determining posterior probability by Bayesian estimation method from prior distribution and observation data of the electromagnetic field, and the current source identifying means includes virtual curved surface identifying means for identifying a virtual curved surface of which corresponding posterior probability attains the highest, among the virtual curved surfaces.

Preferably, the current distribution estimating means includes shallowest virtual curved surface identifying means for identifying a first virtual curved surface closest to the brain surface and having posterior probability attaining a relative maximum, among the plurality of virtual curved surfaces, while successively moving from a virtual curved surface on the side of the brain surface to a deeper side, and the current source identifying means includes localized current distribution identifying means for identifying a localized current distribution corresponding to a point of relative maximum of the current distribution, on the first virtual curved surface, local surface extracting means for separating a plurality of local surfaces each including the localized current distribution, and local surface position identifying means for fixing, among the plurality of local surfaces, local surfaces other than a local surface as an object of identification, moving the local surface as an object of identification in the depth direction, and identifying positions where the posterior probability attains the relative maximum, successively from the side closer to the brain surface.

Preferably, the current distribution estimating means initially estimates the current distribution with a first spatial resolution and thereafter re-estimates the current distribution with a second spatial resolution higher than the first spatial resolution and resolution of the plurality of virtual curved surfaces in the depth direction being improved.

[Embodiments]

Embodiments of the present invention will be described hereinafter with

reference to the figures.

As already described, magnetoencephalography: MEG and electroencephalogram: EEG have been known as methods of monitoring brain activities from the outside. In the following, description will be given mainly focusing on MEG. It is noted, however, that the present invention is also applicable to EEG, when the magnetic field in MEG is replaced by the electric field.

The term “electromagnetic field” originally refers to co-existence of “electric field” and “magnetic field.” In the present specification, however, an expression “observe an electromagnetic field” will be used generally, where the physical amount “to be observed” is an “electric field” or a “magnetic field.”

Fig. 1 is a schematic illustration of an exemplary configuration of an MEG system.

MEG 12 includes an array of multi-channel SQUID flux meter (super sensitive magnetometer), for measuring a magnetic field on the scalp surface of a subject 10. Receiving the result of measurement by MEG 12, a computer system 20 analyzes the result of measurement, and performs a process for estimating the position of a brain current source.

The present invention relates to software processing by computer system 20. It is noted, however, that part of or all of the process may be performed by hardware to increase the speed of processing.

[Principle of brain current source estimation]

Prior to detailed description of the “brain current source estimating method” in accordance with the present invention, the principle and outline of the estimation method of the present invention will be summarized.

(Recovery of electromagnetic field by current distribution on a curved surface)

It is well-known as the principle of electromagnetic shield that when a current source is completely surrounded by a metal surface, electromagnetic field ceases to exist outside the metal surface. When viewed from a different point, this means that



an electromagnetic field identical to that formed by the current source can be formed outside the metal surface by causing an appropriate current flow over the metal surface. On the contrary, the electromagnetic field formed by the current source located outside the metal surface cannot be fully recovered, whatever current is caused to flow over the metal surface. This fact will be referred to as the “principle of electromagnetic field recovery.”

Fig. 2 is a schematic illustration representing an electromagnetic field generated by a current source, observed on an appropriate curved surface.

As can be seen from Fig. 2, when a virtual curved surface is prepared between an observing surface and the current source, it is possible to recover the electromagnetic field formed by the current source on the observing surface by causing an appropriate flow of current on the virtual curved surface, in accordance with the “principle of electromagnetic field recovery” described above.

Fig. 3 is a schematic illustration representing a relation between a current source in the brain and a plurality of virtual curved surfaces.

Referring to Fig. 3, considering that the electromagnetic field formed by the current attenuates in inverse proportion to the square of distance, the expansion of current on the virtual curved surface (virtual curved surface 2) equivalent to the current source becomes wider as the virtual curved surface is further away from the current source. Therefore, the expansion of the current on virtual curved surface 1 is wider than that on virtual curved surface 2.

On a virtual curved surface (virtual curved surface 3) on the side opposite to the observing curved surface with respect to the current source, it is impossible to fully recover the electromagnetic field formed on the observing surface by the current source.

According to the present invention, based on the principle described above, the current source is estimated from the observed data of the electromagnetic field on the observing surface.

(Principle of current source estimation)

Assume that a magnetic field (or an electric field) formed by a current source generated in the brain is observed on an observing surface that is close to the surface of the brain, as shown in Fig. 2.

A virtual curved surface in the brain is considered, and current distribution on the virtual curved surface that recovers the observed magnetic field is calculated. When the virtual curved surface is moved from the surface to the inner side of the brain with the radius made gradually smaller, the expansion of the current distribution recovering the observed magnetic field becomes smaller, and it becomes the smallest when the virtual surface encompasses the true current source. When the virtual curved surface is further moved to be deeper than the current source, the expansion of current distribution on the virtual curved surface comes to be wider again, and the difference between the magnetic field generated by the current and the observed magnetic field also becomes larger.

Accordingly, the depth of the current source can be identified by reviewing the expansion of the current distribution recovering the observed magnetic field and the error in recovery of the magnetic field. Further, by calculating the current distribution on the virtual curved surface at the depth identified in this manner, the expansion of the current source can also be found. The foregoing is the principle of the present invention.

#### (Identification of current source depth by Bayesian estimation)

In order to specifically implement the principle of current source estimation described above, in the present invention, a procedure based on the following probability theory is employed. The procedure will be summarized in the following.

What can be observed by MEG or EEG is several tens of magnetic fields (electric fields) existing near the surface of the brain. In order to approximate the current distribution on the virtual curved surface, lattice points are set on the virtual curved surface, and a current dipole (or an appropriate current source model) is allocated to each lattice point. In order to estimate the current distribution with high

resolution, it is necessary to increase the number of lattice points to increase the density of the lattice points.

When the number of lattice points on the virtual curved surface is increased to be larger than the number of observation points, a unique solution cannot be determined. When estimation points is larger in number than the observation points, the number of parameters to be estimated becomes larger than the number of observed data, and hence, the observed magnetic field would be better recovered even on a virtual curved surface that is positioned deeper than the current source.

In order to cope with such problems, in the present invention, the current distribution on the virtual curved surface is estimated utilizing Bayesian estimation theory. At the time of Bayesian estimation, prior distribution that represents prior information of the current source is used. Specifically, a prior distribution that leads to the smallest possible expansion of current distribution is introduced. Namely, a prior distribution is introduced in which a current dipole on a lattice point of which magnitude cannot be well identified only from the observed data comes to have a magnitude close to zero. This can be realized by introducing hierarchical prior distribution referred to as "Automatic Relevance Determination: ARD" prior distribution.

It is impossible, however, to analytically calculate posterior probability distribution from the ARD prior distribution and observed data. Therefore, in the present invention, variational Bayes method is used as a method of calculating posterior probability distribution by approximation, as will be described later. It is noted that other method of approximation such as Monte Carlo method may be used.

By Bayesian estimation using ARD prior distribution, it becomes possible to obtain a current distribution on the virtual curved surface that recovers the observed data and has smallest possible expansion. Further, by comparing model posterior probabilities when estimations are made using virtual curved surfaces of different depths, the depth of the current source can be identified.

The logarithm of the model posterior probability can be represented as a sum of log-likelihood term and model complexity term. The log-likelihood term becomes larger as recovery error becomes smaller.

The model complexity term becomes larger when the number of effective current dipoles (that is, having a magnitude not smaller than an appropriate threshold) on the lattice points becomes smaller. As already described, the recovery error and the expansion of the current distribution on the virtual curved surface (number of effective current dipoles) become the smallest when the depth of the virtual curved surface matches the current source. Thus, it can be understood that the model posterior probability becomes the largest at this time. In other words, it can be understood that the current source exists on the virtual curved surface at a depth at which the model posterior probability becomes the largest.

In summary, the present invention provides a method of estimating the position of the brain current source, depth direction inclusive, from the observed data of MEG and EEG.

The basic idea of the present invention comes from the fact that an electromagnetic field generated by a current source can be recovered by causing an appropriate current flow over a curved surface existing between the current source and an observing surface, and that the expansion of current distribution on the curved surface becomes smaller as the curved surface comes closer to the current source, as described above. The present invention is characterized in that, based on this idea, the position of the current source including the depth direction is estimated by considering the fact that the model posterior probability becomes the largest when the curved surface encompasses the current source in Bayesian estimation of the current distribution on the curved surface that recovers the observed data, that is, by considering the model posterior probability.

(Where there are a plurality of current sources)

Though description has been made on one current source, the method is also

applicable even when there are a plurality of current sources.

The electromagnetic field generated by a current attenuates in inverse proportion to the square of distance, and therefore, the current source closest to the brain surface has the largest influence on the observed magnetic field on the brain surface. Therefore, it is possible to identify the current sources one by one in order, starting from the one closest to the brain surface.

When the virtual curved surface is moved deeper from the brain surface, the model posterior probability attains the relative maximum near a current source closest to the brain surface (which will be referred to as the first current source). When there are two or more current sources, there will be a plurality of local sets of current dipoles corresponding in number to the current sources, in the current distribution on the virtual curved surface.

The local set of current dipoles is referred to as localized current distribution. A local surface including individual localized current distribution is separated and moved in the depth direction to find the model posterior probability. When the local surface that corresponds to the first current source is moved, the model posterior probability attains to the relative maximum at the depth of the first current source. When other local surfaces are moved, however, the model posterior probability never attains to the relative maximum at the depth of the first current. Thus, the position of the first current source, that is, the position of the current source closest to the brain surface can be identified.

In order to find the second deepest current source, the local surface corresponding to the first current source is fixed, and the depths of the remaining local surfaces are aligned and gradually made deeper. Then the model posterior probability attains the relative maximum at the second deepest current source. When the individual local surface is moved in the depth direction again, the model posterior probability attains to the relative maximum at the depth of the second current source, only when the local surface corresponding to the second current source is moved. In

this manner, the position of the second current source can be identified. The third and the following current sources can also be identified in the similar manner.

The method is advantageous over the method in which the depth of individual local surface is moved independently, in that the time for computation can significantly be reduced.

(Method in which resolution is increased gradually)

According to the method of estimating brain current source of the present invention, it is possible to identify position of each of the current sources starting from the one closest to the brain surface in the above described manner, and in addition, it is possible to gradually increase the resolution of current source estimation.

First, a position of a current source is roughly estimated with a low resolution (with a small number of lattice points on the virtual curved surface and a small number of sample points in the depth direction). In this stage, the position of a local surface corresponding to each current source is approximately determined.

Next, estimation is made with higher resolution. At this time, the area of the local surface has become smaller as compared with the original virtual curved surface, and hence the resolution is naturally higher when the same number of lattice points is used. Accuracy in estimating the current source position can be improved by increasing the resolution in the depth direction as well. If the current distribution is further localized when the resolution is made higher, it is possible to estimate again with local surface made smaller and the resolution made still higher.

On the contrary, if the expansion of current distribution does not much vary even when the resolution is improved, it means that the current source expands wide. In this manner, the resolution can be adjusted in accordance with how the current source expands.

[Specific procedure of current source estimation]

In the following, specific procedure for identifying the position of a “brain current source” will be described in detail, in accordance with the outline above.

[(I) Preparation for current source estimation]

First, preparation for the process procedure for estimating the current source will be described.

Specifically, for the estimation of current source, the following procedures must be taken in advance.

(I-1) Determination of the shape of virtual curved surface and current model

(I-2) Further, in order to estimate the virtual current distribution while moving the virtual curved surface, it is necessary to determine sample points on the virtual curved surface and sample points in the depth direction.

(I-3) Further, as will be described in detail later, it is necessary to determine in advance parameters to designate the distribution shape of hierarchical prior distribution for estimating current distribution as initial values.

In the following, the aforementioned procedure of (I-1) Determination of the shape of virtual curved surface and current model will be described in grater detail.

(I-1-1) Determination of the shape of virtual curved surface

The simplest shape of the virtual curved surface is obtained by regarding the brain as a hemisphere and assuming various hemispheres of different radii to be the virtual curved surfaces.

When a location where existence of a brain current is highly likely such as the cerebral cortex has been known in advance by other measuring methods such as Magnetic Resonance Imaging: MRI, the shape of the virtual curved surface may be determined based on such information.

In this case, the shapes of virtual curved surfaces having different depths may generally differ. It is necessary, however, to determine the shapes not to intersect with each other.

(I-1-2) Determination of current model

As a current model on the virtual curved surface, let us consider a current dipole model. It is also possible to consider other current models.

Consider appropriate lattice points (sample points)  $\{X_n | n=1, \dots, N\}$  on the virtual curved surface. Assume a current dipole of which current intensity is  $j_n$  on each lattice point. Here, the magnetic field formed by the current dipole  $j_n$  at a lattice point  $X_n$  on an observation point  $Y_i$  ( $i=1, \dots, I$ ) on the brain surface is given by the following expression.

$$\mu \frac{j_n \times (Y_i - X_n)}{|Y_i - X_n|^3}$$

Here,  $\mu$  represents magnetic permeability, and by way of example, for a vector  $X_n$ , the expression  $|X_n|$  represents the absolute value of vector  $X_n$ .

Here, the magnetic field formed by the current dipole  $\{j_n | n=1, \dots, N\}$  of the virtual curved surface on an observation point  $Y_i$  ( $i=1, \dots, I$ ) is represented by the following equation.

$$B(Y_i) = \sum_{n=1}^N \mu \frac{j_n \times (Y_i - X_n)}{|Y_i - X_n|^3}$$

Assuming that the direction of the magnetic field observed at the observation point  $Y_i$  is a vector  $S_{i,c}$  ( $c=1, \dots, C$ ), component  $B_{i,c}$  in the direction of vector  $S_{i,c}$  of the magnetic field at this point can be given as

$$B_{i,c} = \sum_{n=1}^N \mu \frac{(j_n \times (Y_i - X_n)) \cdot S_{i,c}}{|Y_i - X_n|^3}$$

Further, when a local gradient of a magnetic field is to be measured as a magnetic field to be observed, a differentiation of the equation above by  $Y_i$  will be observed.

When the direction of a current dipole at a lattice point  $X_n$  (position vector) is restricted, the current dipole can be represented by the following equation, with a possible independent direction of the current dipole being  $b_{n,d}$  ( $d=1, \dots, D$ ). In this equation, a case where  $D = 3$  corresponds to a case where there is no restriction on the direction.



$$\mathbf{j}_n = \sum_{d=1}^D \mathbf{j}_{n,d} \cdot \mathbf{b}_{n,d}$$

In summary, a magnetic field formed by the current dipole at a lattice point  $\{\mathbf{X}_n \mid n=1, \dots, N\}$  of the virtual curved surface on the observation point  $\mathbf{Y}_i$  can be given as

$$\mathbf{B}_{i,c} = \sum_{n=1}^N \sum_{d=1}^D \mathbf{j}_{n,d} \mathbf{G}(\mathbf{i}, \mathbf{c}; \mathbf{n}, \mathbf{d})$$

$$\mathbf{G}(\mathbf{i}, \mathbf{c}; \mathbf{n}, \mathbf{d}) = \mu \frac{(\mathbf{b}_{n,d} \times (\mathbf{Y}_i - \mathbf{X}_n)) \cdot \mathbf{S}_{i,c}}{|\mathbf{Y}_i - \mathbf{X}_n|^3}$$

Here,  $\mathbf{j}_{n,d}$  is an independent component of the current dipole at the lattice point  $\mathbf{X}_n$ . Further, the function  $\mathbf{G}(\mathbf{i}, \mathbf{c}; \mathbf{n}, \mathbf{d})$  represents the component in  $\mathbf{S}_{i,c}$  direction of the magnetic field formed by the current dipole  $\mathbf{b}_{n,d}$  at the lattice point  $\mathbf{X}_n$  on the observation point  $\mathbf{Y}_i$ .

The problem of estimating current distribution may be considered as a problem of estimating a current distribution on the virtual curved surface  $\{\mathbf{j}_{n,d} \mid n=1, \dots, N; d=1, \dots, D\}$  from the observed magnetic field  $\{\mathbf{B}_{i,c} \mid i=1, \dots, I; c=1, \dots, C\}$ .

The measured value of the magnetic field at the observation point described above may be given by the following matrix expression.

$$\mathbf{B} = \mathbf{G} \cdot \mathbf{J}$$

$$\mathbf{B} = (\mathbf{B}_{i,c} \mid i=1, \dots, I; c=1, \dots, C) : (I \times C) \text{ dimensional vector}$$

$$\mathbf{J} = (\mathbf{j}_{n,d} \mid n=1, \dots, N; d=1, \dots, D) : (N \times D) \text{ dimensional vector}$$

$$\mathbf{G} = (\mathbf{G}(\mathbf{i}, \mathbf{c}; \mathbf{n}, \mathbf{d}) \mid i=1, \dots, I; c=1, \dots, C; n=1, \dots, N; d=1, \dots, D) : (I \times C) \times (N \times D) \text{ dimensional matrix}$$

(Current source probability model)

With the current model determined in this manner, the following “current source probability model” is introduced for such current distribution estimation.

(I-1-3) Current source probability model

A probability model for the current model on the virtual curved surface described above will be considered as follows. It is assumed that the observed

magnetic field is represented as a sum of the magnetic field formed by the current distribution  $\mathbf{J}$  on the virtual curved surface and the observation noise. Further, it is assumed that the observation noise is represented as a sum of a bias component irrespective of a measurement site and Gaussian noise having an independent variance  $\sigma^2$  at each measuring point.

Specifically, the observed magnetic field is considered as

$$\mathbf{B} = \mathbf{G} \cdot \mathbf{J} + \xi$$

$$\mathbf{J} = (\mathbf{J}_{\text{virtual curved surface}}, \mathbf{J}_0)$$

$$\mathbf{J}_{\text{virtual curved surface}} = (j_{n,d} \mid n = 1, \dots, N; d = 1, \dots, D)$$

**$\mathbf{J}_0$ : Bias component of noise**

$$\mathbf{G} = (G(i, c; n, d) \mid i = 1, \dots, I; c = 1, \dots, C; n = 1, \dots, N; d = 1, \dots, D)$$

$$G(i, c; 0) \equiv 1$$

$$\xi = (\xi_{i,c} \mid i = 1, \dots, I; c = 1, \dots, C)$$

**: Gaussian noise with each component having independent variance  $\sigma^2$**

The probability distribution for the current model may be considered as follows.

First, a virtual curved surface at a specific depth, or a set of local surfaces with the depth of each local surface identified, will be represented by  $\mathbf{M}$ . When a current distribution  $\mathbf{J}$  on the virtual curved surface  $\mathbf{M}$  is given, the probability  $P(\mathbf{B} \mid \mathbf{J}, \beta, \mathbf{M})$  that the observed magnetic field is  $\mathbf{B}$  is represented by the following equation, where  $\beta = 1/\sigma^2$ .

$$P(\mathbf{B} \mid \mathbf{J}, \beta, \mathbf{M}) = \exp\left[-\frac{1}{2}\beta|\mathbf{B} - \mathbf{G} \cdot \mathbf{J}|^2 + \frac{1}{2}(I \cdot C)\log(\beta/2\pi)\right]$$

$$\beta = 1/\sigma^2$$

(I-1-4) Hierarchical prior distribution

As already described, ARD hierarchical prior distribution will be used as the prior distribution for the current distribution  $\mathbf{J}$  on the virtual curved surface  $\mathbf{M}$ .

The prior distribution for the current distribution  $\mathbf{J}$  before observation

(probability of  $J$  being realized) is represented by the following equation, under the assumption of ARD hierarchical prior distribution.

$$P_0(J | \alpha, \beta, M) = \exp \left[ -\frac{1}{2} \beta \sum_{n=1}^N \alpha_n \left( \sum_{d=1}^D j_{n,d} \right)^2 + \frac{D}{2} \sum_{n=1}^N \log(\beta \alpha_n / 2\pi) - \frac{1}{2} \beta \alpha_0 j_0^2 + \frac{1}{2} \log(\beta \alpha_0 / 2\pi) \right]$$

$$P_0(\beta | \tau, M) = \Gamma(\beta | 1/\tau, \gamma_{\beta 0})$$

Here,  $\Gamma(\dots)$  represents gamma distribution, which is defined below. In the expression below,  $\Gamma(\gamma_0)$  is a gamma function, which is also defined below.

$$\Gamma(\beta | b, \gamma_0) = \frac{1}{\beta} (\gamma_0 \beta / b)^{\gamma_0} \frac{1}{\Gamma(\gamma_0)} e^{-\gamma_0 \beta / b}$$

$$\Gamma(\gamma_0) = \int_0^{\infty} dt t^{\gamma_0-1} e^{-t}$$

Further,  $\alpha$  and  $\tau$  are hyper parameters introduced to model the current distribution  $J$  and prior distribution for inverse variance of noise  $\beta$ . Hierarchical prior distributions  $P_0(\alpha | M)$  and  $P_0(\tau | M)$  for  $\alpha$  and  $\tau$  are

$$P_0(\alpha | M) = \prod_{n=1}^N \Gamma(\alpha_n | a, \gamma_{\alpha 0})$$

$$P_0(\tau | M) = \Gamma(\tau | \bar{\tau}_0, \gamma_{\tau 0})$$

In the equations above, a value for each parameter for  $\alpha$  and  $\tau$  will be described in detail later.

#### (I-1-5) Bayesian estimation

When data  $B$  of a magnetic field is observed, the posterior probability distribution  $P(J|B, M)$  that the current distribution is  $J$  can be calculated in the following manner, using Bayesian theorem.

$$P(J|B, M) = \int d\beta d\alpha d\tau P(J, \beta, \alpha, \tau | B, M)$$

Here, the posterior probability distribution  $P(J, \beta, \alpha, \tau | B, M)$  is given as

$$P(\mathbf{J}, \beta, \alpha, \tau | \mathbf{B}, M) = \frac{P(\mathbf{B} | \mathbf{J}, \beta, M) P_0(\mathbf{J} | \alpha, \beta, M) P_0(\beta | \tau, M) P_0(\alpha | M) P_0(\tau | M)}{P(\mathbf{B} | M)}$$

$$P(\mathbf{B} | M) = \int d\mathbf{J} d\beta d\alpha d\tau P(\mathbf{B} | \mathbf{J}, \beta, M) P_0(\mathbf{J} | \alpha, \beta, M) P_0(\beta | \tau, M) P_0(\alpha | M) P_0(\tau | M)$$

Using this posterior probability distribution, an expected value  $E[\mathbf{J} | \mathbf{B}, M]$  of current distribution is given as

$$\mathbf{J} = E[\mathbf{J} | \mathbf{B}, M] = \int d\mathbf{J} d\beta d\alpha d\tau P(\mathbf{J}, \beta, \alpha, \tau | \mathbf{B}, M) \mathbf{J}$$

Further,  $P(\mathbf{B} | M)$  represents marginal likelihood of the virtual curved surface model  $M$ . When the depth of a current source is estimated, a number of models having different depths are compared. At this time, it is assumed that there is no prior information about the depth. Specifically, in the following, it is assumed that  $P(M) = \text{constant}$ .

When the observation data  $\mathbf{B}$  is given, the probability that the model  $M$  is a true model, that is, the model posterior probability  $P(M | \mathbf{B})$ , is in proportion to the model marginal likelihood  $P(\mathbf{B} | M)$  under the assumption described above, and hence, the following relation holds.

$$P(M | \mathbf{B}) \propto P(\mathbf{B} | M)$$

#### (I-1-6) Variational Bayes method

It is generally impossible to analytically calculate the model marginal likelihood when the probability model and the hierarchical prior distribution are given.

Therefore, as a method of calculating by approximation the model marginal likelihood, variational Bayes method is used. It is possible to use other method of approximation, such as Monte Carlo method and Laplacian approximation.

The “variational Bayes method” will be briefly outlined, and specific procedure will be described later.

In order to calculate a true posterior distribution  $P(J, \beta, \alpha, \tau | B, M)$  by approximation, a trial posterior distribution  $Q(J, \beta, \alpha, \tau)$  is considered.

Closeness between the two probability distributions  $P(J, \beta, \alpha, \tau | B, M)$  and  $Q(J, \beta, \alpha, \tau)$  can be calculated by using K-L distance given by the following expressions.

$$\begin{aligned}
 & KL(P||Q) \\
 &= \int dJ d\beta d\alpha d\tau Q(J, \beta, \alpha, \tau) \log \left[ \frac{Q(J, \beta, \alpha, \tau)}{P(J, \beta, \alpha, \tau | B, M)} \right] \\
 &= \log P(B | M) - F(Q) \geq 0 \\
 & F(Q) \equiv \int dJ d\beta d\alpha d\tau Q(J, \beta, \alpha, \tau) \times \\
 & \quad \log \left[ \frac{P(B | J, \beta, M) P_0(J | \alpha, \beta, M) P_0(\beta | \tau, M) P_0(\alpha | M) P_0(\tau | M)}{Q(J, \beta, \alpha, \tau)} \right]
 \end{aligned}$$

The K-L distance attains to zero only when the two distributions are equal to each other, and otherwise it always assumes a positive value.

When a free energy  $F(Q)$  for the trial posterior distribution  $Q$  is defined in the expression above, the following inequality results.

$$F(Q) \leq \log P(B | M)$$

Specifically, the distribution  $Q(J, \beta, \alpha, \tau)$  that maximizes the free energy  $F(Q)$  becomes equal to the true posterior distribution  $P(J, \beta, \alpha, \tau | B, M)$ , and at this time, the free energy is equal to the marginal log-likelihood.

According to variational Bayes method, the form of function  $Q(J, \beta, \alpha, \tau)$  is restricted to the following form, to maximize the free energy.

$$Q(J, \beta, \alpha, \tau) = Q_J(J, \beta) Q_\alpha(\alpha, \tau)$$

By alternately repeating the step of fixing the second term  $Q_\alpha$  on the right side of the equation above and maximizing  $F(Q)$  with respect to the first term  $Q_J$  on the right side and the step of fixing the first term  $Q_J$  and maximizing  $F(Q)$  with respect to the second term  $Q_\alpha$ , a distribution  $Q^*$  is obtained that attains the relative maximum of free energy  $F(Q)$ .

[(II) Procedure of current source estimation]

A specific procedure for estimating the current source after the preparation above will be described hereinafter with reference to the figures.

Fig. 4 is a flow chart representing an overall procedure of the brain current source position estimating method in accordance with the present invention.

Referring to Fig. 4, first, when the process of estimating a position of a brain current source starts (step S100), values of parameters for designating the shape of hierarchical prior distribution for estimating the current distribution and an initial value of a variable to be estimated are determined (step S102).

Thereafter, initial estimation of the current source is performed, using an initial resolution, so as to extract candidates of the current source (step S104).

Then, among the current source candidates extracted in this manner, a position of a current source that is closest to the brain surface is identified (step S106).

Thereafter, depths of other current sources are identified successively (step S108).

After the positions of current sources are identified with the initial resolution in the above-described manner, re-estimation of the positions of the current sources is performed with the spatial resolution increased (step S110), and the process ends (step S112).

Processes of respective steps of Fig. 4 will be described in greater detail in the following.

(II-1) Initial estimation of current source using initial resolution (extraction of current source candidates)

Fig. 5 is a flow chart representing the process of step S104 among the steps shown in Fig. 4, that is, the process of initial estimation of the current source using an initial resolution.

Referring to Fig. 5, first, sample points in the depth direction with the initial resolution are determined to be  $\{R_k | k=1, \dots, K\}$ . Current distribution is estimated for the virtual curved surface at each depth  $R_k$ . Further, based on the current distribution estimated in this manner, posterior probability for each depth  $R_k$  is calculated. The

posterior probability corresponds to the free energy value, which will be described later (step S202).

For the current distribution at the depth  $R_M$  at which the posterior probability calculated in this manner becomes the highest, a relative maximum point of current intensity is found (step S204).

Further, a local surface that encompasses each relative maximum point is determined. Assuming that there are  $L$  local surfaces, each local surface will be the candidate of localized current source (step S206).

In the following, the process of step S102 of Fig. 4 and the process of step S202 of Fig. 5 that follows, will be described in greater detail.

(II-1-1) Determination of parameter values for designating shape of hierarchical prior distribution for estimating current distribution and initial values of variables to be estimated

As described above, estimation of a current source is performed using variational Bayes method. Therefore, the process of step S102 shown in Fig. 4 is performed in the following manner, with the application of variational Bayes method.

The parameters designating the shape of hierarchical prior distribution are determined as follows.

$$\gamma_{\beta 0} = 1 \quad (\text{more generally, } 0 < \gamma_{\beta 0} \leq 1)$$

$$\gamma_{\tau 0} = 1 \quad (\text{more generally, } 0 < \gamma_{\tau 0} \leq 1)$$

$$\gamma_{\alpha 0} = 0.1 \quad (\text{more generally, } 0 < \gamma_{\alpha 0} \leq 1)$$

$$\bar{\tau}_0 = \kappa_{\tau} \cdot V_{ar}(\mathbf{B}), \quad \kappa_{\tau} = 1 \quad (\text{more generally, } \kappa_{\tau} \sim 1)$$

$$V_{ar}(\mathbf{B}) = \frac{1}{I \cdot C} \sum_{i=1}^I \sum_{c=1}^C (B_{i,c} - \bar{B})^2$$

$$\bar{B} = \frac{1}{I \cdot C} \sum_{i=1}^I \sum_{c=1}^C B_{i,c}$$

$$a = \kappa_{\alpha} \cdot \frac{1}{N} Tr(\mathbf{G}' \cdot \mathbf{G}), \quad \kappa_{\alpha} = 0.1 \quad (\text{more generally, } 0 < \kappa_{\alpha} \leq 1)$$

$$\tilde{N} = D \cdot N + 1$$

Further, based on the equations above, each variable is initialized in the following manner.

$$\gamma_{\beta} = \frac{1}{2} \mathbf{I} \cdot \mathbf{C} + \gamma_{\beta 0}$$

$$\gamma_{\tau} = \gamma_{\tau 0} + \gamma_{\beta 0}$$

$$\gamma_{\alpha} = \gamma_{\alpha 0} + \frac{1}{2} \mathbf{D}$$

$$\overline{\alpha}_n = a$$

$$\overline{\tau} = \overline{\tau}_0$$

$$\Sigma_{\mathbf{G}} = \mathbf{G}' \cdot \mathbf{G}$$

(II-1-2) Specific process of variational Bayes method for estimating current distribution

(1) Calculation of expected values of parameters  $\mathbf{J}$ ,  $\beta$  (M-step process)

Here, expected values of parameters  $\mathbf{J}$  and  $\beta$  are calculated. By this process, the free energy  $F(\mathbf{Q})$  for  $\mathbf{Q}_{\mathbf{J}}$  is maximized.

By defining a diagonal matrix  $\mathbf{A}$  as follows,  $\mathbf{Q}_{\mathbf{J}}$  is derived in accordance with the following equations. In the following equations, an expected value of a variable is represented by the variable name with “—” attached thereabove.

$$A(n, d; n', d') = \delta_{nn'} \delta_{dd'} \overline{\alpha}_n \quad (n, n' = 1, \dots, N; d, d' = 1, \dots, D)$$

$$A(n, d; 0) = A(0; n', d') = 0$$

$$A(0; 0) = \overline{\alpha}_0$$

$$\Sigma = \Sigma_{\mathbf{G}} + \mathbf{A}$$

$$\overline{\mathbf{J}} = \Sigma^{-1} \cdot \mathbf{G}' \cdot \mathbf{B}$$

$$\overline{\beta} = \gamma_{\beta} \left[ \frac{1}{2} \left| \mathbf{B} - \mathbf{G} \cdot \overline{\mathbf{J}} \right|^2 + \frac{1}{2} \overline{\mathbf{J}}' \mathbf{A} \overline{\mathbf{J}} + \gamma_{\beta 0} \overline{\tau} \right]^{-1}$$

$$\mathbf{Q}_{\mathbf{J}}(\mathbf{J}, \beta) = \mathbf{Q}_{\mathbf{J}}(\mathbf{J} | \beta) \mathbf{Q}_{\beta}(\beta)$$



$$Q_J(\mathbf{J} | \beta) = \exp\left[-\frac{1}{2}\beta(\mathbf{J} - \bar{\mathbf{J}})' \Sigma(\mathbf{J} - \bar{\mathbf{J}}) + \frac{1}{2}\log|\Sigma| + \frac{1}{2}\tilde{N}\log(\beta/2\pi)\right]$$

$$Q_\beta(\beta) = \Gamma(\beta | \bar{\beta}, \gamma_\beta)$$

(2) Calculation of expected values of hyper parameters, that is, calculation of expected values of parameters  $\alpha$ ,  $\tau$  (process for H-step)

Following the M step, expected values of hyper parameters  $\alpha$  and  $\tau$  are calculated. In this step, a process is performed to maximize the free energy  $F(Q)$  for  $Q_\alpha$ .

The procedure can be represented as

$$\bar{\alpha}_n = \gamma_\alpha [\gamma_{\alpha_0}^{-1} + \frac{1}{2} \beta \sum_{d=1}^D \bar{j}_{n,d}^2 + \sum_{d=1}^D (\Sigma^{-1})(n, d; n, d)]^{-1} \quad (n=1, \dots, N)$$

$$\bar{\alpha}_0 = (\gamma_{\alpha_0} + \frac{1}{2}) [\gamma_{\alpha_0}^{-1} + \frac{1}{2} \beta \bar{j}_0^2 + (\Sigma^{-1})(0; 0)]^{-1}$$

$$\bar{\tau} = \gamma_\tau [\gamma_{\tau_0} \bar{\tau}_0^{-1} + \gamma_{\beta_0} \bar{\beta}]^{-1}$$

$$Q_\alpha(\alpha, \tau) = \Gamma(\tau | \bar{\tau}, \gamma_\tau) \Gamma(\alpha_0 | \bar{\alpha}_0, \gamma_{\alpha_0} + \frac{1}{2}) \prod_{n=1}^N \Gamma(\alpha_n | \bar{\alpha}_n, \gamma_\alpha)$$

(3) Calculation of free energy

Using  $Q_J$  and  $Q_\alpha$  calculated through the M step and H step as described above, the free energy is calculated in the following manner.

$$F = LP + H_J + H_\beta + H_\alpha + H_\tau$$

$$LP = -\frac{1}{2} \overline{\beta} |B - G \cdot \overline{J}|^2 - \frac{1}{2} \text{Tr} \Sigma^{-1} \Sigma_a + \frac{1}{2} (I \cdot C) (\langle \log \beta \rangle - \log 2\pi)$$

$$\langle \log \beta \rangle = \log \overline{\beta} + \psi(\gamma_\beta) - \log \gamma_\beta$$

$$\psi(\gamma) \equiv \frac{d(\log \Gamma(\gamma))}{d\gamma} \quad \psi: \text{digamma function}$$

$$H_J = -\frac{1}{2} [\text{Tr} \Sigma^{-1} A - \log |\Sigma^{-1} A| - \tilde{N}] - \frac{1}{2} \overline{\beta} \overline{J^T A J}$$

$$H_\beta = \Phi(\gamma_\beta, \gamma_{\beta 0}) + \gamma_{\beta 0} [\langle \log \beta \rangle + \langle \log \tau \rangle - \overline{\tau} \overline{\beta} + 1]$$

$$\langle \log \tau \rangle = \log \overline{\tau} + \psi(\gamma_\tau) - \log \gamma_\tau$$

$$\Phi(\gamma, \gamma_0) \equiv (\log \Gamma(\gamma) - \gamma \psi(\gamma) + \gamma) - (\log \Gamma(\gamma_0) - \gamma_0 \log \gamma_0 + \gamma_0)$$

$$H_\tau = \Phi(\gamma_\tau, \gamma_{\tau 0}) + \gamma_{\tau 0} [\langle \log \tau \rangle - \log \overline{\tau}_0 - \overline{\tau} \overline{\tau}_0^{-1} + 1]$$

$$H_\alpha = \sum_{n=1}^N [\Phi(\gamma_\alpha, \gamma_{\alpha 0}) + \gamma_{\alpha 0} (\langle \log \alpha_n \rangle - \log a - \overline{\alpha}_n a^{-1} + 1)]$$

$$+ \Phi(\gamma_{\alpha 0} + \frac{1}{2}, \gamma_{\alpha 0}) + \gamma_{\alpha 0} (\langle \log \alpha_0 \rangle - \log a - \overline{\alpha}_0 a^{-1} + 1)$$

$$\langle \log \alpha_n \rangle = \log \overline{\alpha}_n + \psi(\gamma_\alpha) - \log \gamma_\alpha \quad (n=1, \dots, N)$$

$$\langle \log \alpha_0 \rangle = \log \overline{\alpha}_0 + \psi(\gamma_{\alpha 0} + \frac{1}{2}) - \log(\gamma_{\alpha 0} + \frac{1}{2})$$

In this manner, the process from the M step to calculation of free energy described above is repeated until the value of free energy F converges. The value of free energy F(Q) after convergence gives an approximation of marginal log-likelihood  $\log P(B|M)$ .

Further, model log-posterior probability differs only by the constant from  $\log P(B|M)$ , and therefore, the model having the maximum model posterior probability is the same as the model of which free energy is the highest, in accordance with the above-described approximation.

By the above-described procedure, posterior probability for the depth  $R_k$  can be calculated. By performing the processes of steps S204 and S206 of Fig. 5 described above accordingly, it is possible to find candidates of current sources localized to respective local surfaces.

## (II-2) Identification of current source closest to the brain surface

Next, the process of step S106 of Fig. 4, that is, the process for identifying the current source closest to the brain surface among the candidates of current sources found in the manner as described above, will be described.

Fig. 6 is a flow chart representing a process for identifying a current source closest to the brain surface.

First, as the initial value, the value of a variable  $l$  is set to 1 (step S302). Then, the variable  $l$  is compared with a possible maximum value  $L$  of variable  $l$  (step S304), and when the variable  $l$  is not larger than the maximum value  $L$ , the process proceeds to step S306, and when the variable  $l$  exceeds the maximum value  $L$ , the process proceeds to step S324 (step S304). Specifically, the process from step S306 to step S322 is repeated from  $l=1$  to  $l=L$ .

In step S306, depth of a local surface other than the  $l$ th local surface is fixed at the depth  $R_M$  calculated in step S204 of Fig. 5.

The value of variable  $k$  is set to 1 (step S308). Thereafter, the variable  $k$  is compared with a possible maximum value  $K$  of variable  $k$  (step S310), and when the variable  $k$  is not larger than the maximum value  $K$ , the process proceeds to step S312, and when the variable  $k$  exceeds the maximum value  $K$ , the process proceeds to step S320.

In step S312, the depth of the  $l$ th local surface is first determined to be  $R_k$ .

Thereafter, current distribution is estimated for the set of  $L$  local surfaces (step S314).

Thereafter, the posterior probability (free energy) for this arrangement of the local surfaces is calculated (step S316). By incrementing the value of variable  $k$  by only 1 (step S318), the process returns to step S310.

The process is performed for each of the local surfaces having the depths from  $k=1$  to  $k=K$ , and then, the depth  $R_M(l)$  of the  $l$ th local surface that provides the highest posterior probability is calculated (step S320). By incrementing the value of variable  $l$

only by 1 (step S322), the process returns to step S304.

In this manner, among the depths  $R_M(l)$  of the local surfaces calculated for each variable  $l$ ,  $l$  closest to the brain surface (shallow) is detected, which is denoted by  $l_1$  (step S324).

Through the steps described above, it follows that the  $l_1$ th local surface corresponds to the current source closest to the brain surface, the initial estimated value of the depth thereof is calculated as  $R_M(l_1)$ , and the process terminates (step S326).

(II-3) Identification of depth of current source corresponding to each local surface

Figs. 7 and 8 are flow charts representing a process of step S108 of Fig. 4, that is, a process for identifying depth of a current source corresponding to each local surface.

Referring to Fig. 7, the value of a variable  $s$  is set to 1 as an initial value (step S402). Thereafter, the variable  $s$  is compared with a possible maximum value  $L$  of variable  $s$  (step S404), and when the variable  $s$  is not larger than the maximum value  $L$ , the process proceeds to step S406, and when the variable  $s$  exceeds the maximum value  $L$ , the process proceeds to step S434 (step S404). Specifically, the process from step S406 to step S432 is repeated from  $s=1$  to  $s=L$ .

In step S406, when the depths of local surfaces identified so far are represented as  $\{R_M(l_1), \dots, R_M(l_s)\}$ , the depths of these local surfaces are fixed at  $\{R_M(l_1), \dots, R_M(l_s)\}$ , respectively (step S406).

First, it is assumed that  $l$  is not equal to any of  $\{l_1, \dots, l_s\}$ , and that  $l$  belongs to a set of  $\{1, \dots, L\}$  (step S408). Then, whether all possible values are considered as the value of variable  $l$  or not is determined (step S410), and if all the possible values have been considered, the process proceeds to step S430. Otherwise, the process proceeds to step S412.

In step S412, the depth of a local surface that is different from the  $l$ th local surface and not any of  $\{l_1, \dots, l_s\}$  is fixed at  $R_M$ .

The value of variable  $k$  is set to 1 (step S414). Thereafter, the variable  $k$  is compared with a possible maximum value  $K$  of variable  $k$  (step S416), and when the variable  $k$  is not larger than the maximum value  $K$ , the process proceeds to step S418, and when the variable  $k$  exceeds the maximum value  $K$ , the process proceeds to step S426. Specifically, the process from step S418 to step S424 is repeated from  $k=1$  to  $k=K$ .

In step S418, the depth of the  $l$ th local surface is set to  $R_k$ .

Thereafter, for the set of  $L$  local surfaces, current distribution is estimated (step S420).

Further, posterior probability (free energy) for this arrangement of the local surfaces is calculated (step 422).

Referring to Fig. 8, in step S426, after the process to  $k=K$  is finished in the above-described manner, the depth  $R_M(l)$  of the  $l$ th local surface attaining the highest posterior probability is calculated (step S426).

Then, other variable  $l$  that is not equal to any of  $\{l_1, \dots, l_s\}$ , belongs to the set of  $\{1, \dots, L\}$  and is not yet processed is selected (step S428), and the process returns to step S410.

Through the above-described steps, among  $R_M(l)$  values corresponding to all the processed variables  $l$ , the value  $l$  that is closest to the brain surface is calculated and denoted by  $l_{s+1}$  (step S430).

Further,  $s$  is replaced by  $s+1$  (step S432), and the process returns to step S404.

When the process ends for all the possible values  $s$ , identification of the depths of current sources corresponding to respective local surfaces is finished (step S434).

#### (II-4) Re-estimation of current source with increased resolution

Figs. 9 and 10 are flow charts representing the process of step S110 shown in Fig. 4, that is, the process for re-estimating a position of a current source with higher spatial resolution.

Referring to Figs. 9 and 10, first, numbers of local surfaces corresponding to the

current sources estimated using the initial resolution are re-numbered so that the surfaces have the numbers 1, 2, 3, ..., L starting from the one closest to the brain surface (step S502). Then, corresponding to the expansion of current distribution on each local surface, the local surface is made smaller (step S504).

The depth of the local surface  $R_M(l)$  calculated by the process up to step S108 of Fig. 4 is denoted as  $R_M^{old}(l)$  (step S506).

New resolution and search width in the depth direction are respectively represented as  $\Delta R$  and  $(K_L \bullet \Delta R)$ . Further, resolution of lattice points on the local surface is also increased (step S508).

The value of a variable l is set to 1 as an initial value (step S510). Thereafter, the variable l is compared with a possible maximum value L of variable l (step S512), and when the variable l is not larger than the maximum value L, the process proceeds to step S514, and when the variable l exceeds the maximum value L, the process proceeds to step S534 (step S512). Specifically, the process from step S514 to step S532 is repeated from  $l=1$  to  $l=L$ .

In step S514, the depth of a local surface  $l'$  other than the  $l$ th local surface is fixed to  $R_M^{old}(l')$ .

Further, the process from step S518 to step S526 below is performed with  $k=0, \pm 1, \dots, \pm K_L$ .

First, the value of variable k is set to 0 (step S516). Thereafter, the absolute value of variable k is compared with the possible maximum absolute value of  $K_L$  of variable k (step S518), and when the absolute value of variable k is not larger than the maximum value  $K_L$ , the process proceeds to step S520, and when the absolute value of variable k exceeds the maximum value  $K_L$ , the process proceeds to step S528 (step S518).

In step S520, the depth of the  $l$ th local surface is set to  $(R_M^{old}(l) + k \bullet \Delta R)$ .

Thereafter, for the set of L local surfaces, current distribution is estimated using the present resolution (step S522).

Further, posterior probability (free energy) for this arrangement of the local surfaces is calculated (step S524). Then, the value  $k$  is set to the next one of  $\{\pm 1, \dots, \pm K_L\}$ , and the process returns to step S518.

After the above-described process is performed until  $k=\pm K_L$ , the value  $k$  that provides the highest posterior probability is calculated in step S528, which value is denoted by  $k_M$ .

Then,  $R_M^{\text{old}}(l)$  is replaced by  $R_M^{\text{old}}(l) + k_M \bullet \Delta R$  (step S530). The value of variable  $l$  is incremented by only 1 (step S532), and the process returns to step S512.

When the above-described process has been performed until the value of variable  $l$  attains to the maximum value  $L$  and the resolution has reached the final resolution (step S534), the process is terminated (step S538).

When the resolution is not yet the final resolution (step S534), the resolution of the lattice points on the local surface and the resolution in the depth direction are increased (step S536), and the process returns to step S510.

By the “method of estimating brain current source” as described above, it becomes possible to estimate the position of a brain current source, including the position in the depth direction, from observation data of MEG (or EEG). Further, such estimation in the depth direction is applicable even when there are a plurality of current sources. Still further, the method is applicable when the current sources are localized as in the case of current dipoles or when the current source has an expansion. In addition, by the method, it is also possible to estimate how the current source expands.

By additionally performing the process described with reference to Figs. 9 and 10 after the estimation with the initial resolution, it becomes possible to successively increase resolution for estimating a position. This also means that it is possible to review with the scope of search restricted based on physiological findings or the like.

[Result of simulation]

In the following, simulation results will be described, in which current source

positions of an assumed model were estimated in accordance with the method of estimating brain current source described above.

Fig. 11 is a top view of a magnetic field distribution in the radial direction observed on a surface of a hemisphere, assuming that the human brain is a hemisphere having the radius of 10.0 (arbitrary unit).

Fig. 11 shows a magnetic field distribution on a surface of the hemisphere in which a single current source is positioned at a radius of 7.0 from the center, as will be described later. In the simulation that will be discussed below, noise having the S/N ratio of 0.1 is added to the observation data of the magnetic field.

Fig. 12 represents results of initial estimation of current sources using initial resolution.

Fig. 12 shows the result of calculation of current distribution, in which, as described with reference to the process of steps S102 to S104 of Fig. 4, in order to perform initial estimation of the current source using the initial resolution, the depth (radius) is changed stepwise and on the hemisphere of each depth, the current distribution that attains the maximum free energy is calculated in accordance with variational Bayes method.

Fig. 12(a) shows the result where the radius is  $R=5.0$ , 12(b) shows the result where the radius is  $R=6.0$  and 12(c) shows the result where the radius is  $R=7.0$ .

Fig. 13 represents results of initial estimation of current sources using initial resolution, where the radius is larger (that is, closer to the surface of the brain).

Fig. 13(d) shows the result where the radius is  $R=7.5$ , 13(e) shows the result where the radius is  $R=8.0$  and 13(f) shows the result where the radius is  $R=9.0$ .

Fig. 14 represents magnitude of free energy on each virtual hemispherical surface, obtained when current distribution that attains maximum free energy is calculated for virtual hemispherical surfaces at various depths assumed in the brain.

Referring to Fig. 14, it can be understood that the maximum point of free energy exists between the radii of 7 and 8, when calculation is made assuming that the



hemispherical surface as a whole is a virtual curved surface.

As can be seen from Fig. 13(d), one point of relative maximum exists in the current distribution on the virtual hemispherical surface having the radius of  $R=7.5$ .

As the current source is initially estimated using the initial resolution in this manner, on the virtual curved surface having the maximum free energy, a local surface that encompasses the relative maximum point of current distribution is calculated, and the process for identifying the current source is performed on the local surface.

Figs. 15 and 16 represent processes for identifying the current source executed further on a local surface including a point of relative maximum of the current distribution, with the resolution of lattice points on the local surface and the resolution in the depth direction increased.

Figs. 15(a), 15(b) and 15(c) represent current distribution on local surfaces where the radius is  $R=5.0$ ,  $R=6.0$  and  $R=7.0$ , respectively. Similarly, Figs. 16(d), 16(e) and 16(f) represent current distribution where the radius is  $R=7.5$ ,  $R=8.0$  and  $R=9.0$ , respectively.

Fig. 17 represents the resultant free energy calculated with the depth of local surface varied.

Referring to Fig. 17, the free energy as a result of calculation using the local surface has the relative maximum value near the radius of  $R=7$ , and from the result, it is possible to identify that one current source exists at the position of  $R=7$ .

The current distribution of the current source at this time is as shown in Fig. 15(c), and as already described, it can be understood that the current distribution also has the narrowest expansion.

Fig. 18 is a top view of a magnetic field distribution observed on a surface of the brain assumed as a hemisphere, when there are two current sources in the brain.

In the example shown in Fig. 18, it is assumed that the current sources are positioned at the radii of  $R=6.0$  and  $R=8.0$ .

Figs. 19 and 20 represent results of initial estimation of current sources using

initial resolution.

Specifically, Figs. 19 and 20 illustrate the process (step S104) for performing initial estimation of current sources using the initial resolution shown in Fig. 4, when there are two current sources in the brain.

Figs. 19(a), 19(b) and 19(c) represent current distribution on virtual hemispherical surfaces where the radius is  $R=5.0$ ,  $R=6.0$  and  $R=7.0$ , respectively.

Figs. 20(d), 20(e) and 20(f) represent current distribution on virtual hemispherical surfaces where the radius is  $R=7.5$ ,  $R=8.0$  and  $R=9.0$ , respectively.

Fig. 21 represents radius dependency of free energy, when current distribution that attains maximum free energy is calculated for each virtual hemispherical surface of the whole hemispherical surfaces.

As shown in Fig. 21, when the free energy is calculated over the entire hemispherical surface, it is understood that the maximum value of free energy exists between the radii of  $R=7$  and  $R=8$ , that is, near the radius of  $R=7.5$ .

As can be seen from Fig. 20(d), on the virtual hemispherical surface having the radius of  $R=7.5$ , there are two relative maximum points in the current distribution and two local surfaces are determined.

Next, the result of calculation corresponding to the process of step S106 shown in Fig. 4 will be described.

Figs. 22 and 23 illustrate the process for calculating the depth of an  $l$ th local surface  $R_M(l)$  attaining maximum posterior probability, to identify a current source closest to the brain surface.

Therefore, Figs. 22 and 23 represent current distribution when a local surface corresponding to one current source is moved while the other local surface is fixed on a surface that attains the maximum free energy calculated over the entire hemispherical surface.

Figs. 22(a), 22(b) and 22(c) represent current distribution on local surfaces where the radius is  $R=5.0$ ,  $R=6.0$  and  $R=7.0$ , respectively.

Figs. 23(d), 23(e) and 23(f) represent current distribution on local surfaces where the radius is  $R=7.5$ ,  $R=8.0$  and  $R=9.0$ , respectively.

Fig. 24 represents local surface position (radius) dependency of free energy when a virtual local surface is moved as shown in Figs. 22 and 23.

As shown in Fig. 24, when a local surface corresponding to one current source is moved to the position of radius  $R=8$  while the other local surface is fixed on a surface that attains the maximum free energy calculated over the entire hemispherical surface, the free energy is maximized.

Therefore, from the result shown in Fig. 24, it can be seen that the position of the current source closest to the brain surface is at the radius of  $R=8.0$ .

Thereafter, the depth of the other current source is identified.

Here, the depth of the local surface corresponding to one current source is fixed at the radius of  $R=8.0$ , and the depth of the local surface corresponding to the other current source is varied.

Figs. 25 and 26 represent current distribution when one local surface is fixed on a specific surface and a local surface corresponding to the other current source is moved.

Figs. 25(a), 25(b) and 25(c) represent current distribution on local surfaces where the radius is  $R=5.0$ ,  $R=5.5$  and  $R=6.0$ , respectively.

Figs. 26(d), 26(e) and 26(f) represent current distribution on local surfaces where the radius is  $R=6.5$ ,  $R=7.0$  and  $R=7.5$ , respectively.

Fig. 27 represents local surface position (radius) dependency of free energy when a virtual local surface is moved as shown in Figs. 25 and 26.

As can be seen from Fig. 27, here, the free energy attains relative maximum at the position of radius  $R=6$ .

It can be understood that by such a process, even when there are two current sources in the brain, it is possible to identify the depth of each of the current sources.

It should be understood that the embodiments disclosed herein are illustrative and non-restrictive in every respect. The scope of the present invention is defined by

the terms of the claims, rather than the description above, and is intended to include any modifications within the scope and meaning equivalent to the terms of the claims.

[Effects of the Invention]

As described above, according to the brain current source estimating method of the present invention, it is possible to estimate the position of a brain current source including the depth direction, from observation data of MEG or EEG. Such estimation in the depth direction is applicable even when there are a plurality of current sources. Further, the method is applicable where the current sources exist locally as in the case of current dipoles and applicable to a current source that has a certain expansion. Further, it is possible to estimate how the current source expands. In addition, after the estimation with the initial resolution, it is possible to successively increase resolution for estimating a position.

[Brief Description of the Drawings]

Fig. 1 is a schematic illustration of an exemplary configuration of an MEG system.

Fig. 2 is a schematic illustration representing an electromagnetic field generated by a current source, observed on an appropriate curved surface.

Fig. 3 is a schematic illustration representing a relation between a current source in the brain and a plurality of virtual curved surfaces.

Fig. 4 is a flow chart representing an overall procedure of the brain current source estimating method in accordance with the present invention.

Fig. 5 is a flow chart representing a process of initial estimation of the current source using an initial resolution.

Fig. 6 is a flow chart representing a process for identifying a current source closest to the brain surface.

Fig. 7 is a first flow chart representing a process for identifying depth of a current source corresponding to each local surface.

Fig. 8 is a second flow chart representing a process for identifying depth of a

current source corresponding to each local surface.

Fig. 9 is a first flow chart representing a process for re-estimating a position of a current source with higher spatial resolution.

Fig. 10 is a second flow chart representing a process for re-estimating a position of a current source with higher spatial resolution.

Fig. 11 is a top view of a magnetic field distribution observed on a surface of a hemisphere, assuming that the human brain is a hemisphere.

Fig. 12 represents results of initial estimation of current sources using initial resolution.

Fig. 13 represents results of initial estimation of current sources using initial resolution, where the radius is greater (closer to the surface of the brain).

Fig. 14 represents magnitude of free energy on each virtual hemispherical surface, obtained when current distribution that attains highest free energy is calculated.

Fig. 15 is a first diagram representing processes for identifying the current source executed further on a local surface including a point of relative maximum.

Fig. 16 is a second diagram representing processes for identifying the current source executed further on a local surface including a point of relative maximum.

Fig. 17 represents the resultant free energy calculated with the depth of local surface varied.

Fig. 18 is a top view of a magnetic field distribution observed on a surface of the brain assumed as a hemisphere, when there are two current sources in the brain.

Fig. 19 is a first diagram representing results of initial estimation of current sources using initial resolution.

Fig. 20 is a second diagram representing results of initial estimation of current sources using initial resolution.

Fig. 21 represents radius dependency of free energy, when current distribution that attains highest free energy is calculated for each virtual hemispherical surface.

Fig. 22 is a first diagram for illustrating the process for calculating the depth of

an  $l$ th local surface attaining maximum posterior probability, to identify a current source closest to the brain surface.

Fig. 23 is a second diagram for illustrating the process for calculating the depth of an  $l$ th local surface attaining maximum posterior probability, to identify a current source closest to the brain surface.

Fig. 24 represents local surface position (radius) dependency of free energy when a virtual local surface is moved.

Fig. 25 is a first diagram representing current distribution when one local surface is fixed on a specific surface and a local surface corresponding to the other current source is moved.

Fig. 26 is a second diagram representing current distribution when one local surface is fixed on a specific surface and a local surface corresponding to the other current source is moved.

Fig. 27 represents local surface position (radius) dependency of free energy when a virtual local surface is moved.

[Description of the Reference Characters]

10 subject; 12 MEG; and 20 computer system.

FIG.1

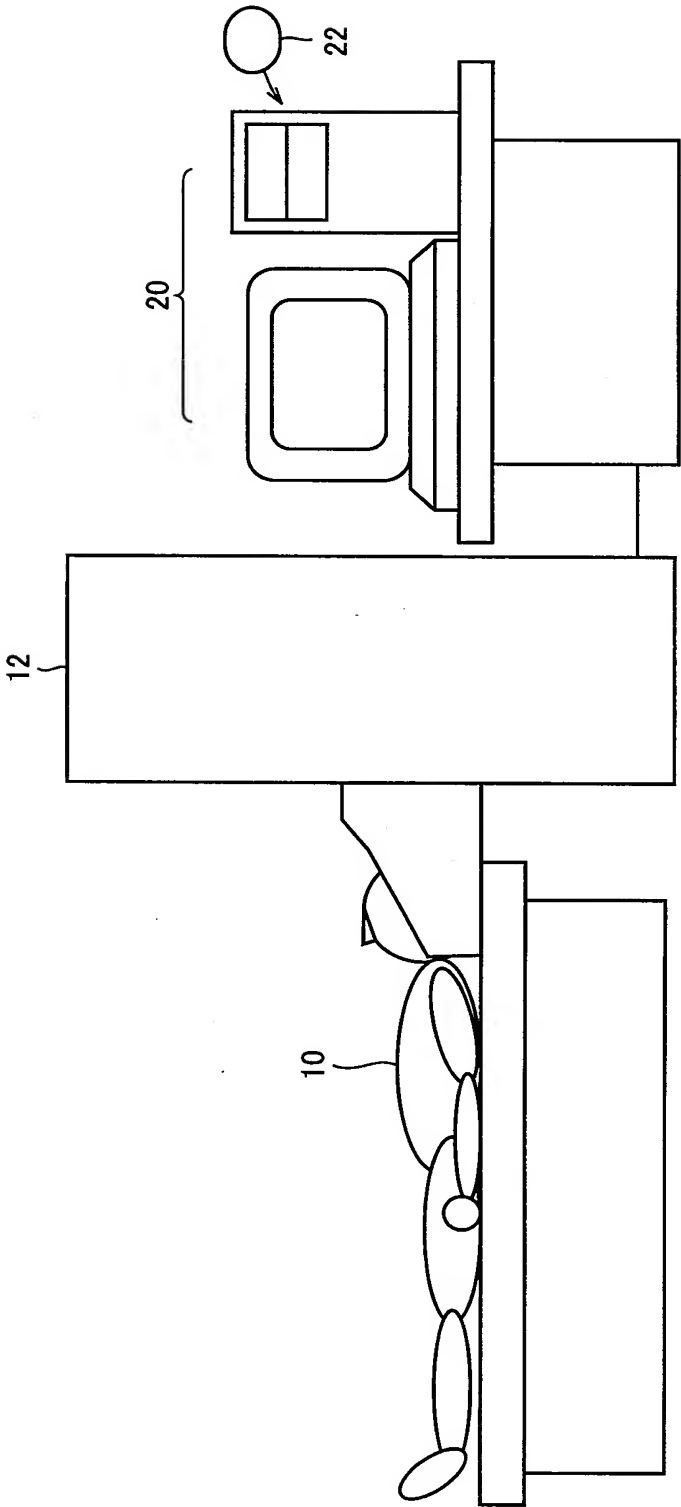


FIG.2

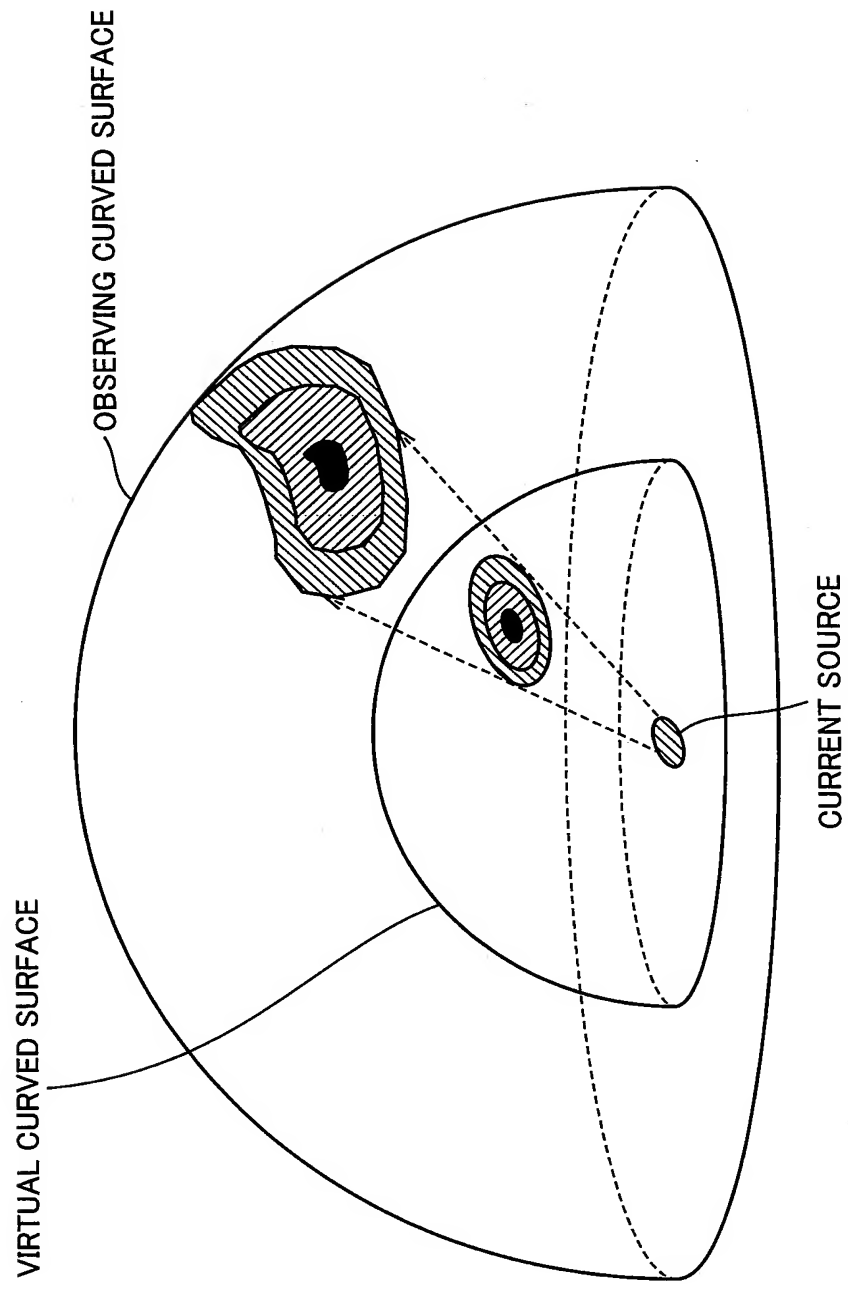




FIG.3

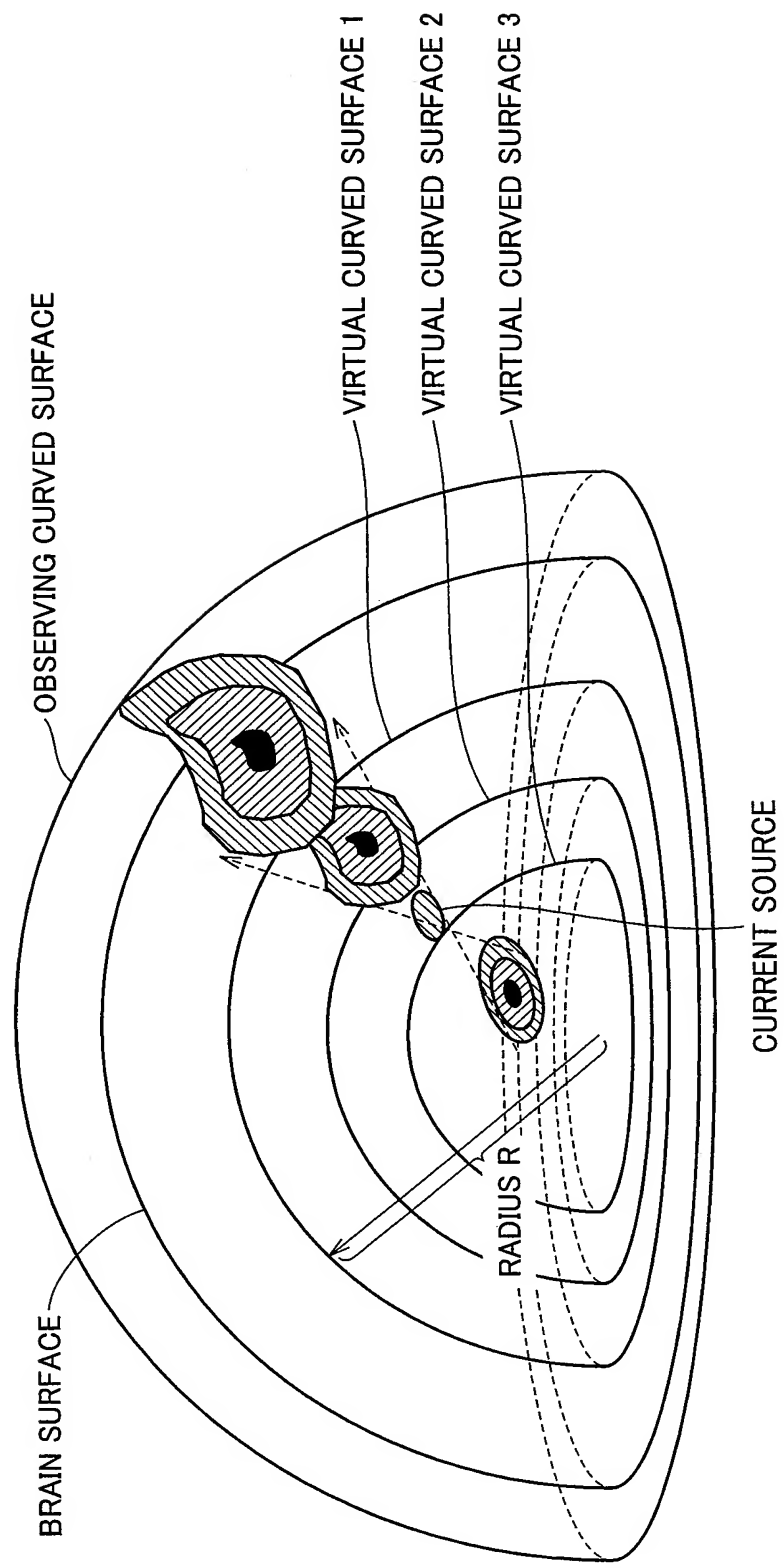


FIG.4

ESTIMATION OF CURRENT SOURCE

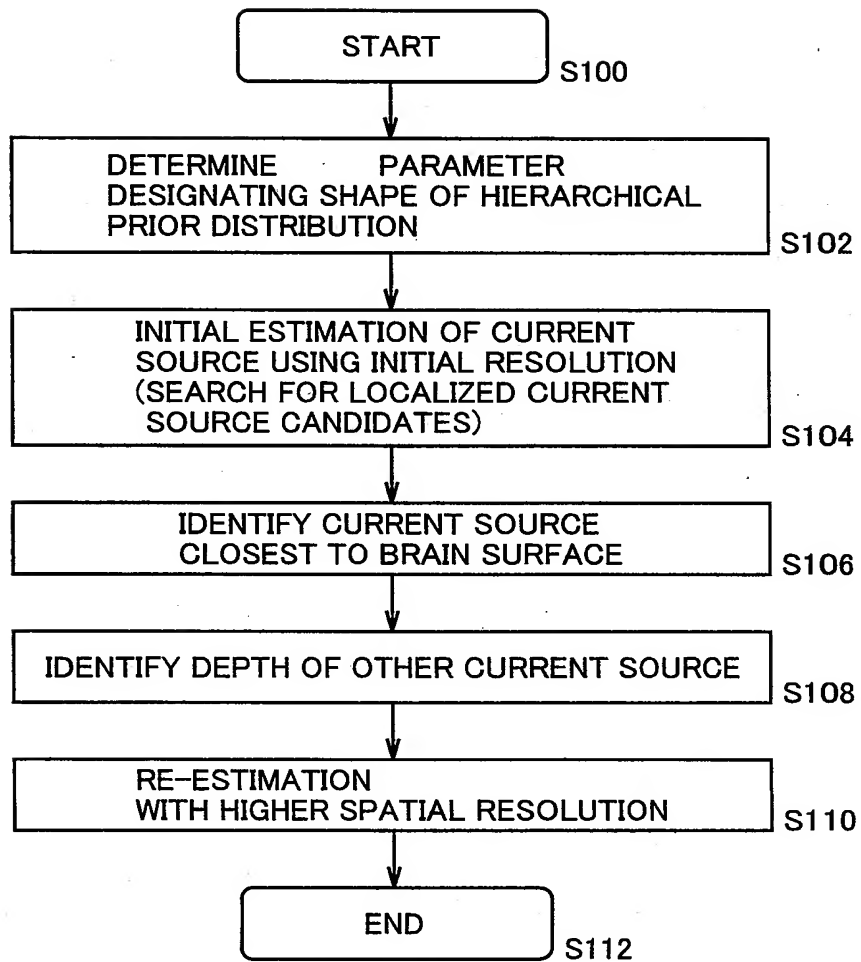


FIG.5

INITIAL ESTIMATION OF  
CURRENT SOURCE

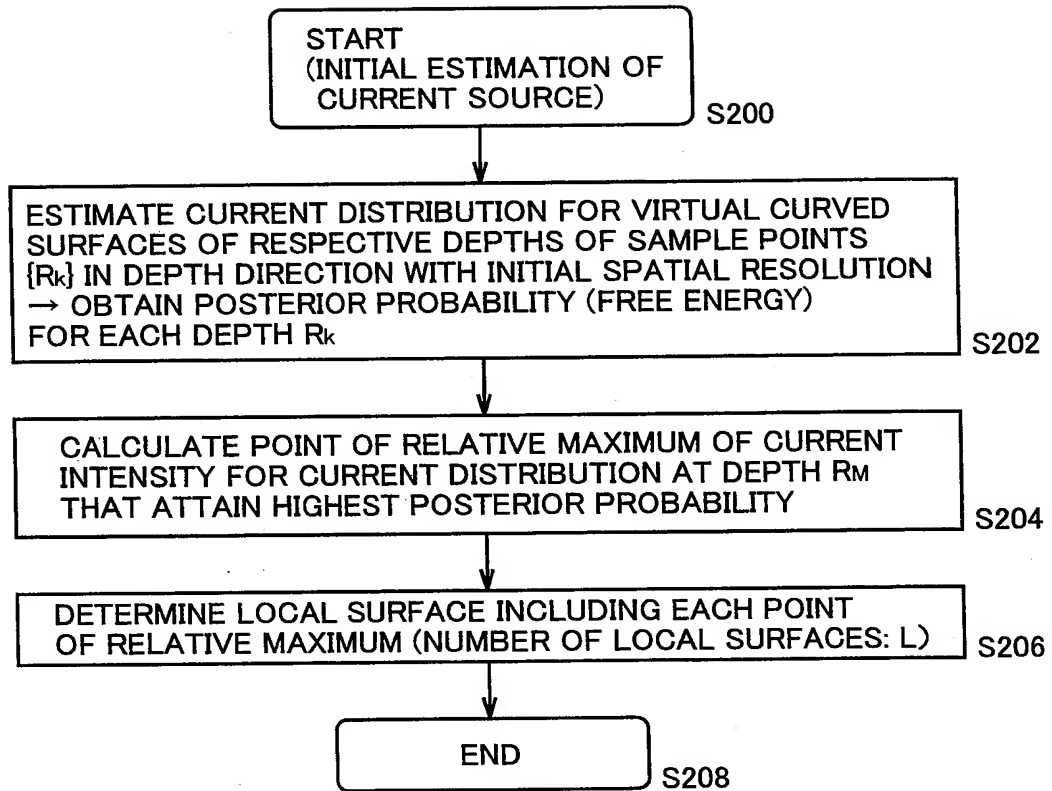


FIG.6

ESTIMATION OF CURRENT  
SOURCE CLOSEST TO  
BRAIN SURFACE

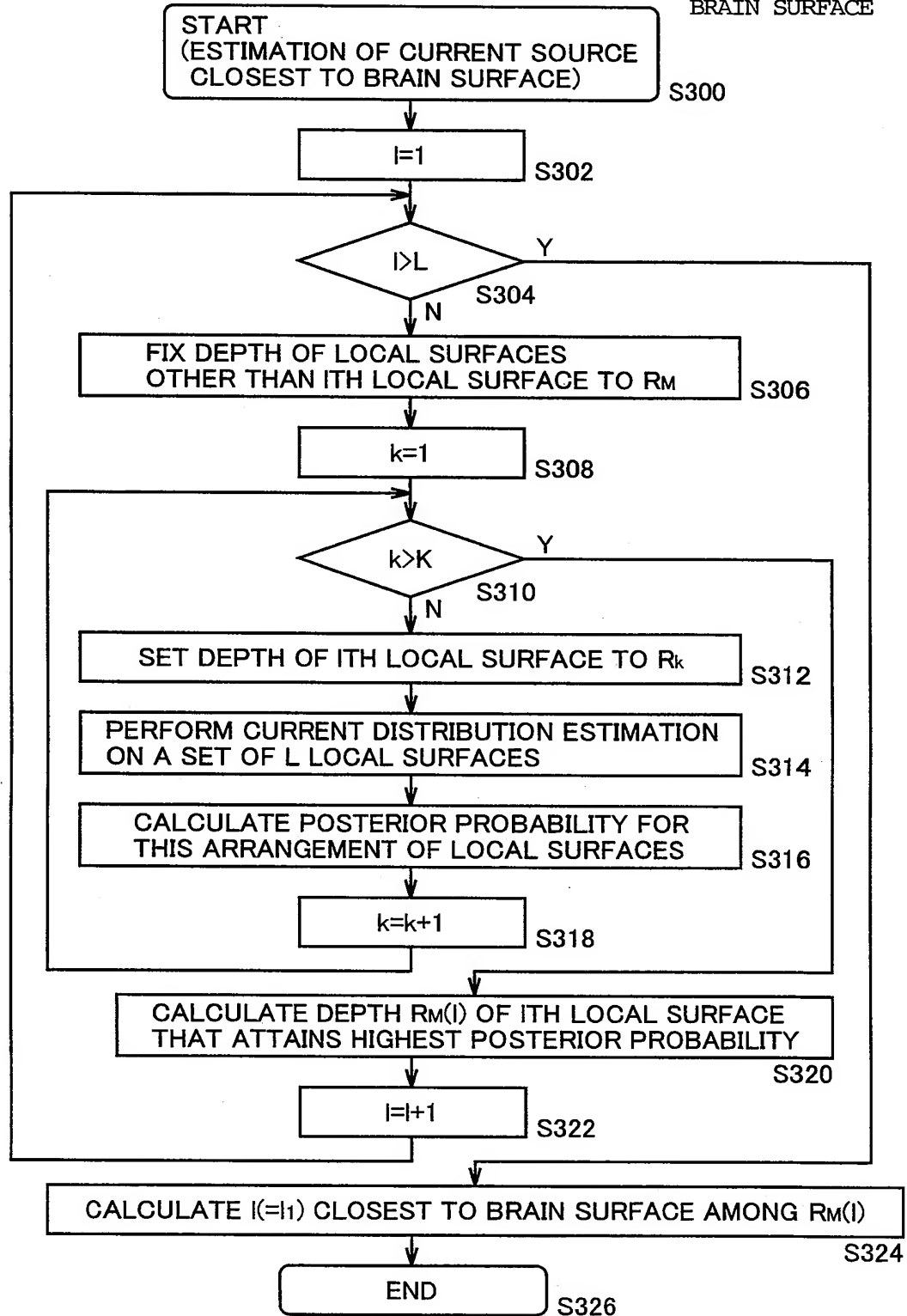


FIG.7

IDENTIFICATION OF DEPTH  
OF CURRENT SOURCE

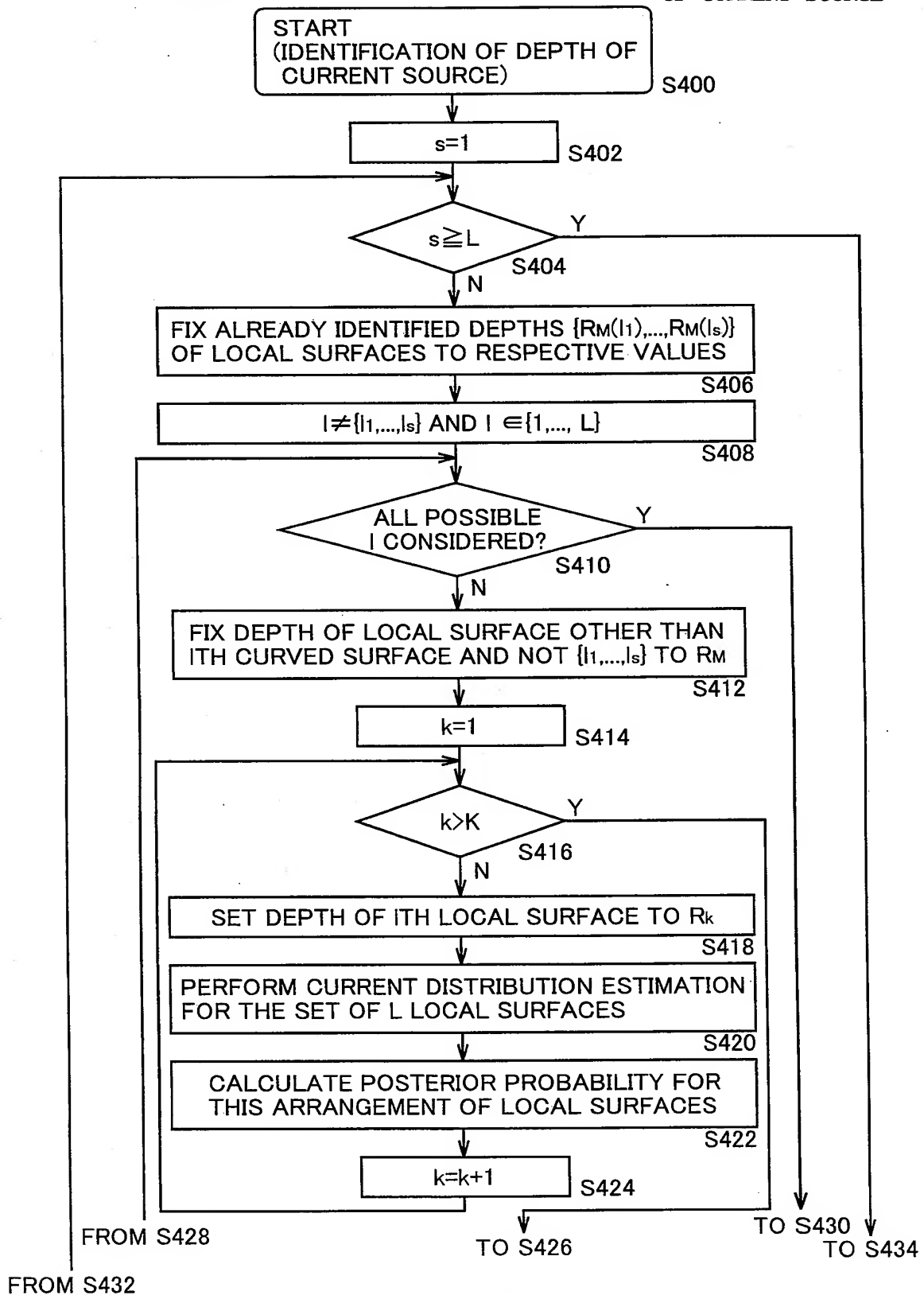


FIG.8

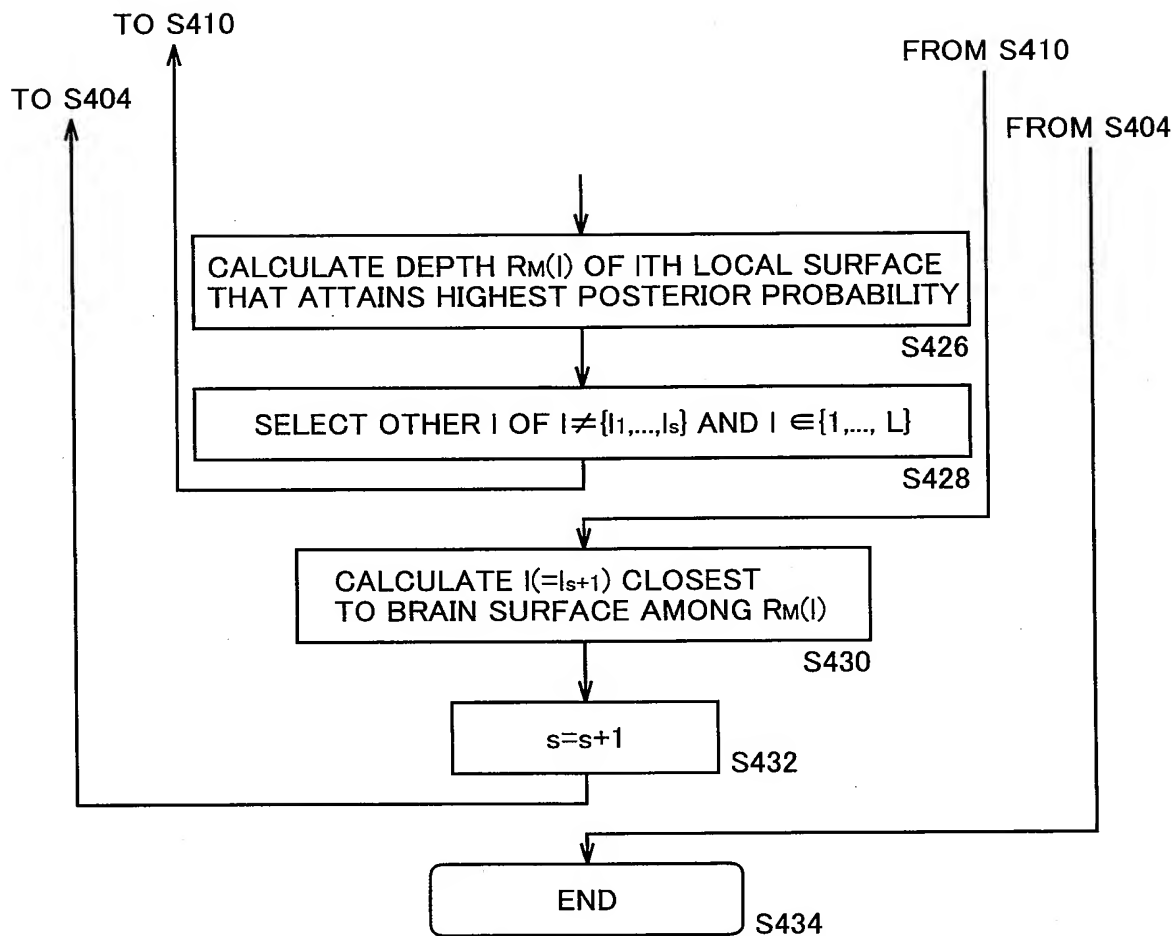


FIG.9

RE-ESTIMATION OF  
CURRENT SOURCE WITH  
HIGHER RESOLUTION

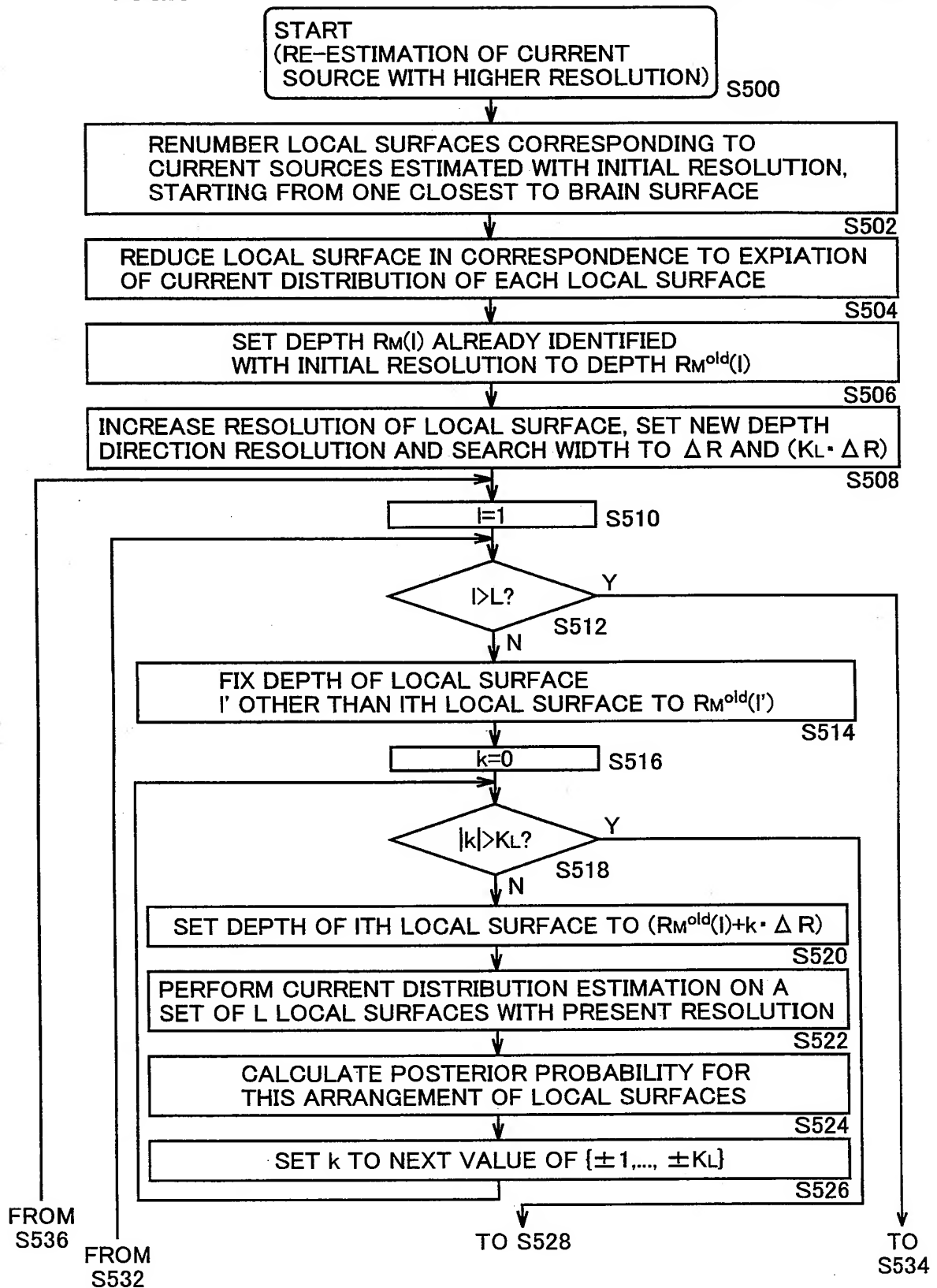


FIG.10

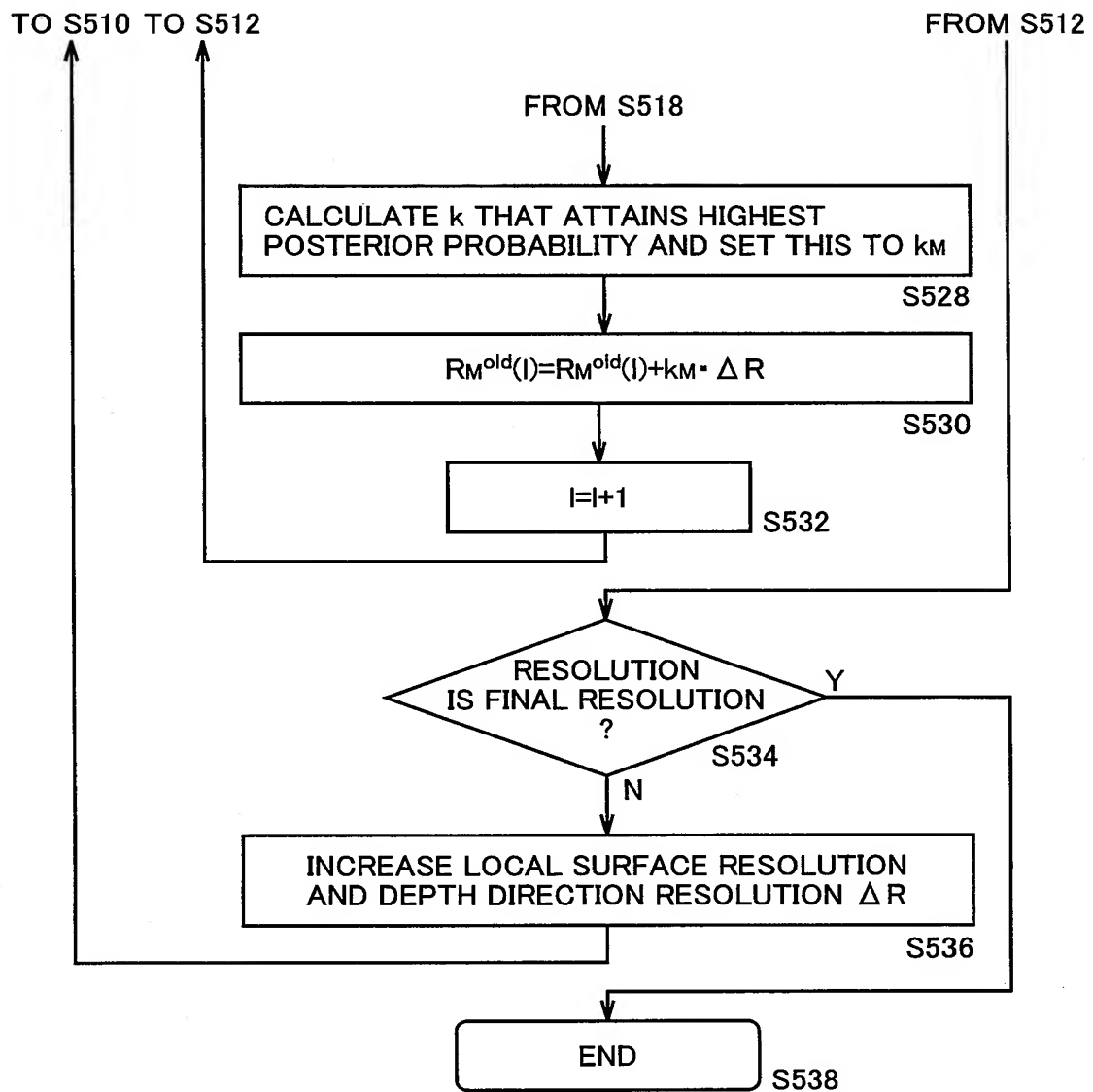




FIG.11

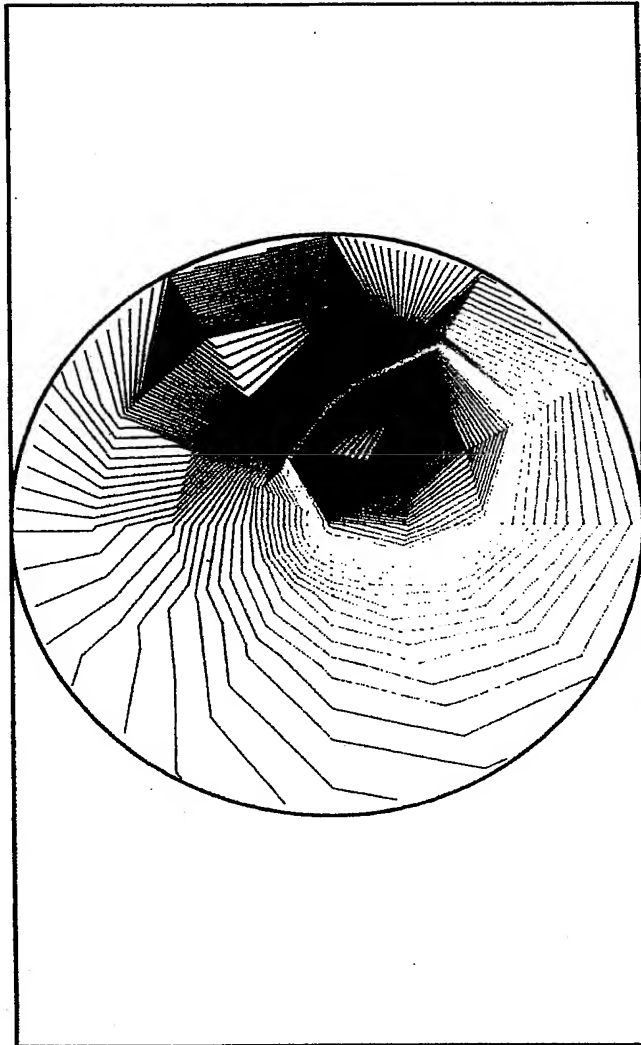


FIG.12(a)

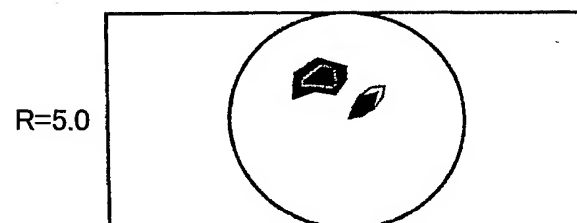


FIG.12(b)

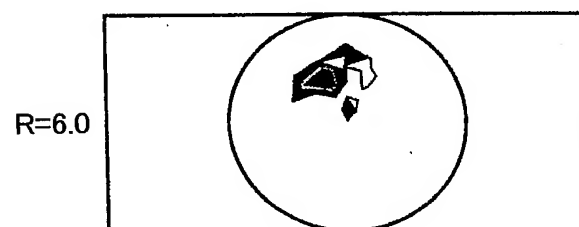


FIG.12(c)

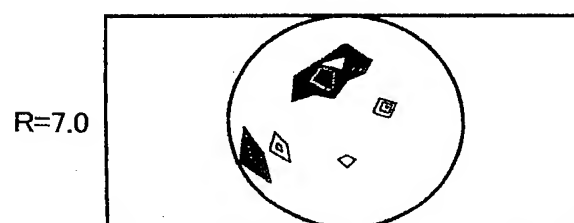


FIG.13(d)

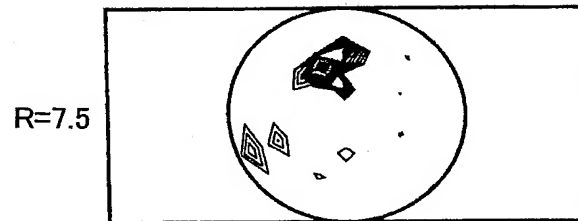


FIG.13(e)

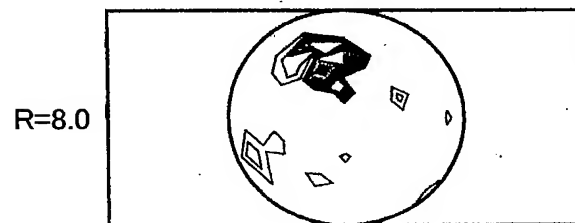


FIG.13(f)

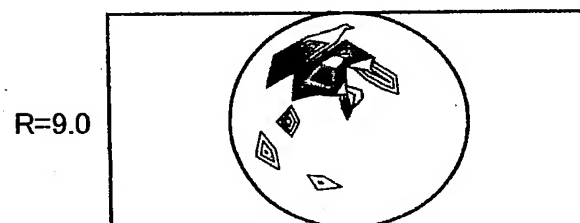


FIG.14

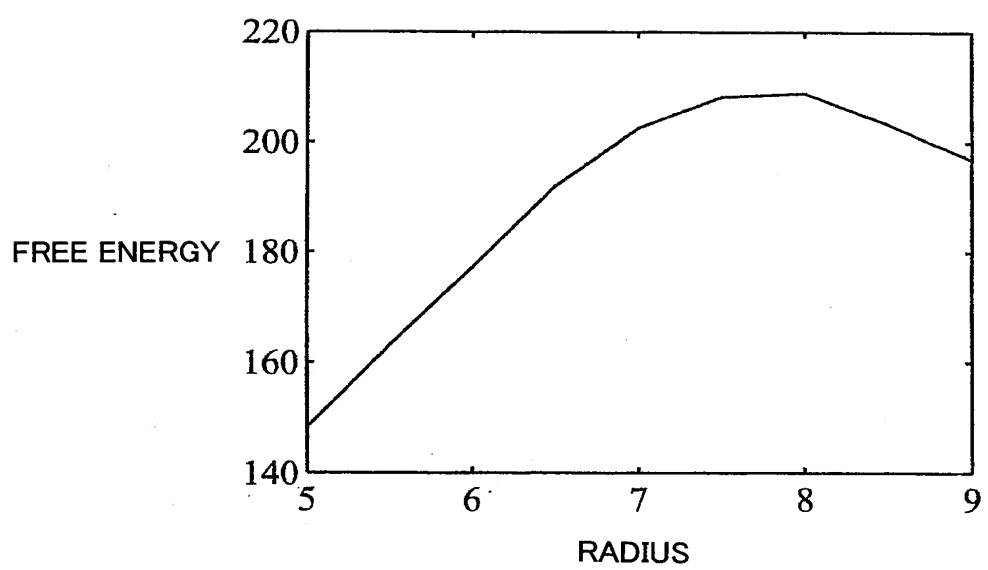


FIG.15(a)

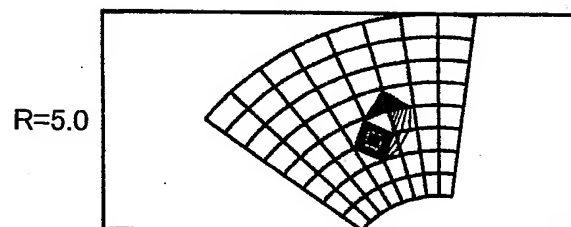


FIG.15(b)

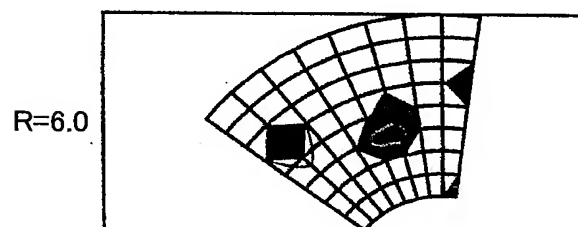


FIG.15(c)

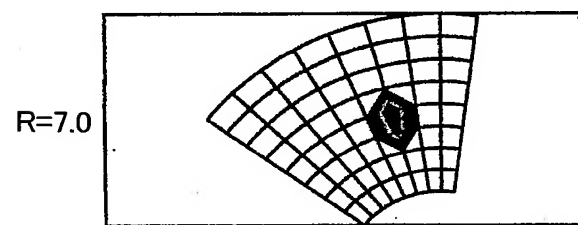


FIG.16(d)

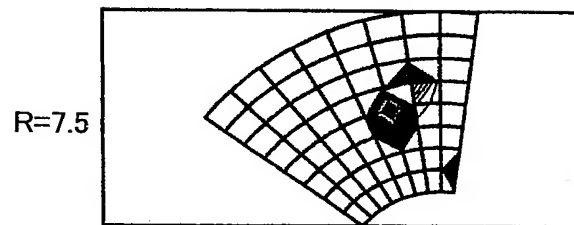


FIG.16(e)

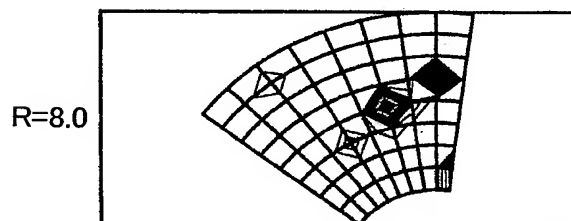


FIG.16(f)

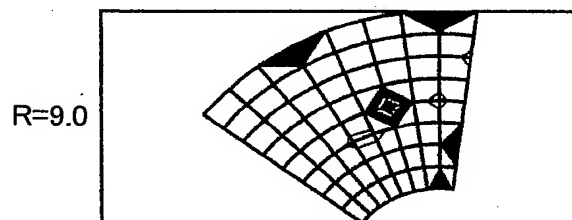


FIG.17

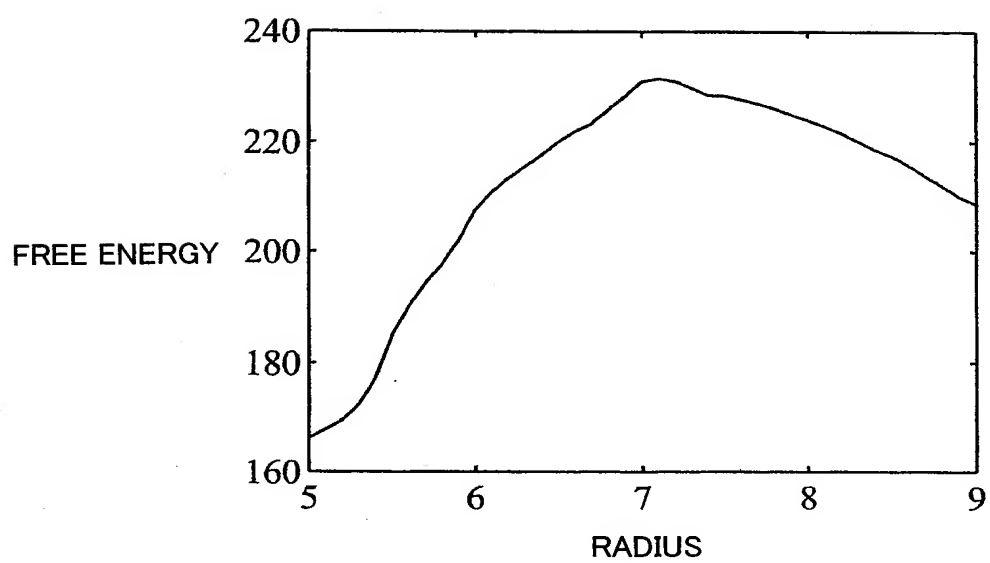


FIG.18

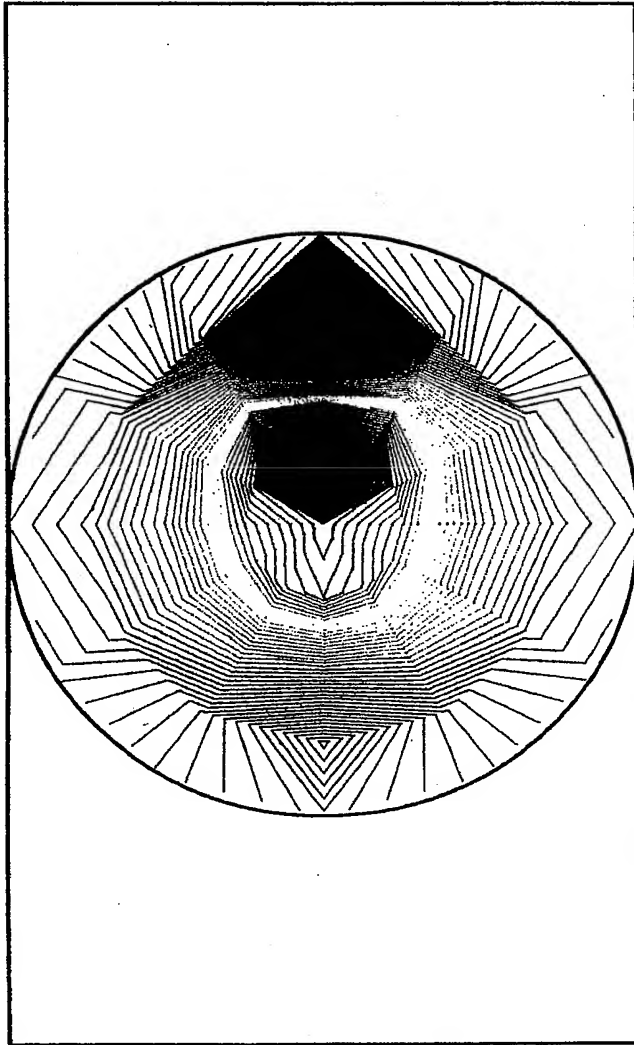




FIG.19(a)

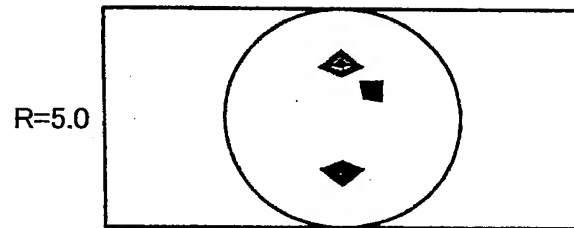


FIG.19(b)

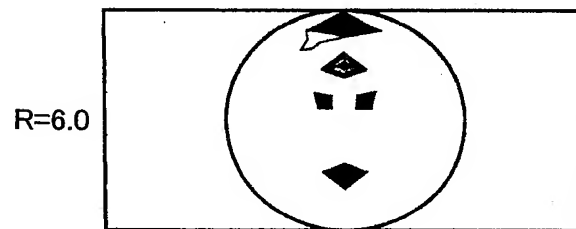


FIG.19(c)

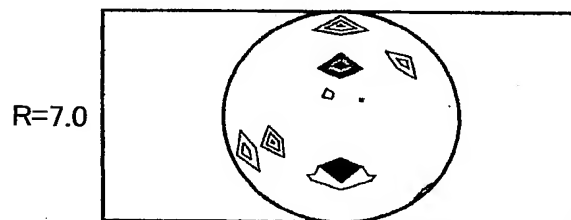


FIG.20(d)

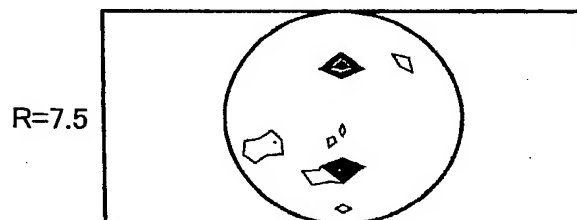


FIG.20(e)

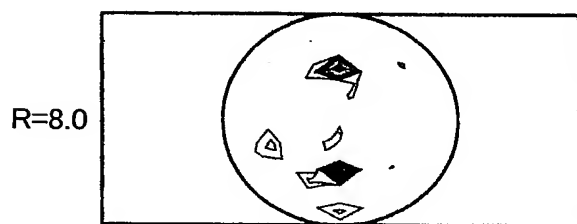


FIG.20(f)

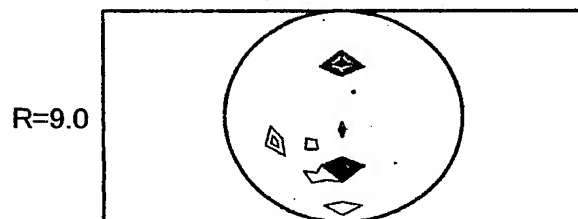


FIG.21

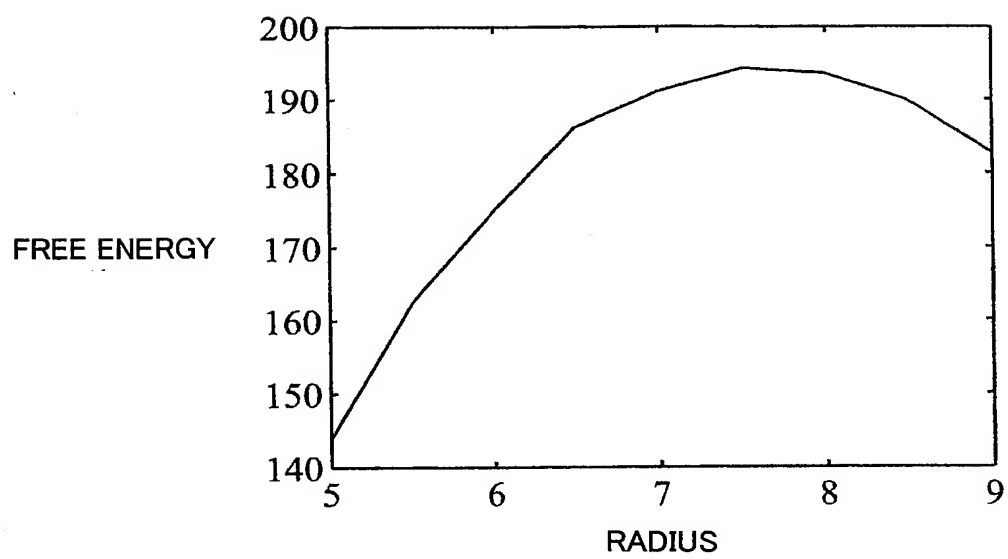


FIG.22(a)

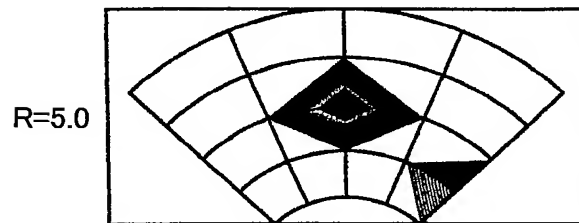


FIG.22(b)

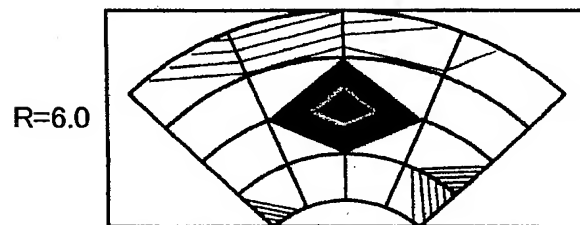


FIG.22(c)

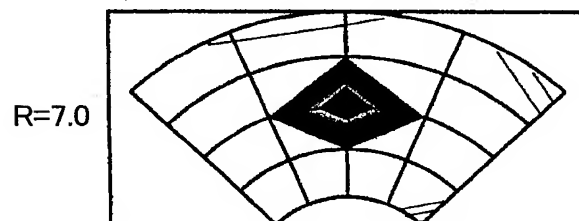


FIG.23(d)

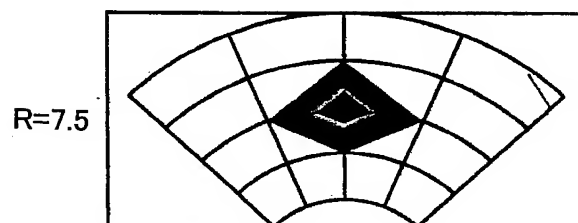


FIG.23(e)

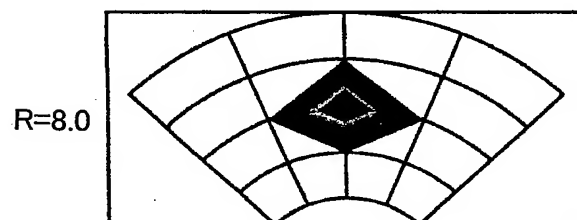


FIG.23(f)

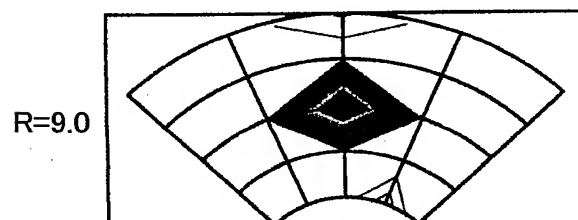


FIG.24

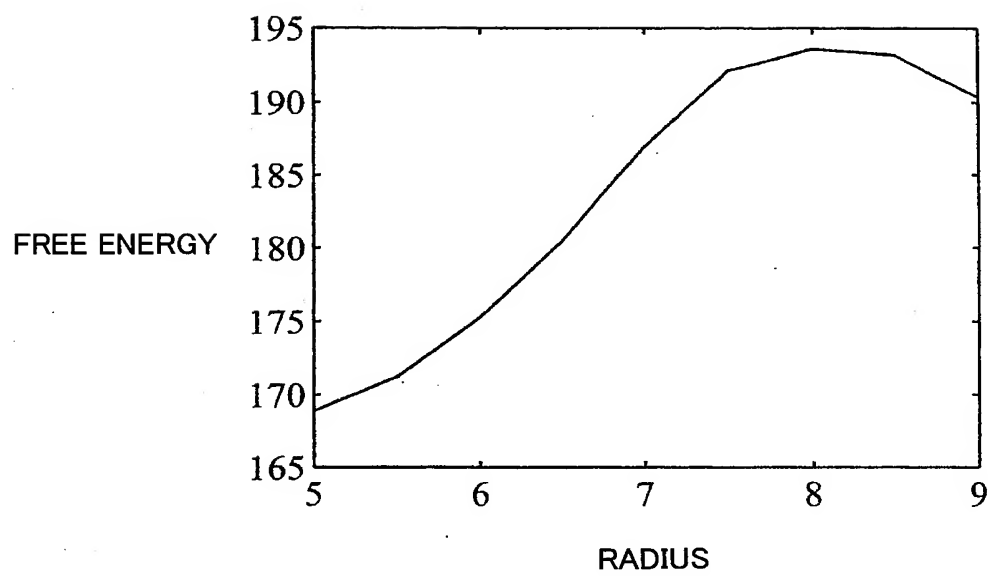


FIG.25(a)

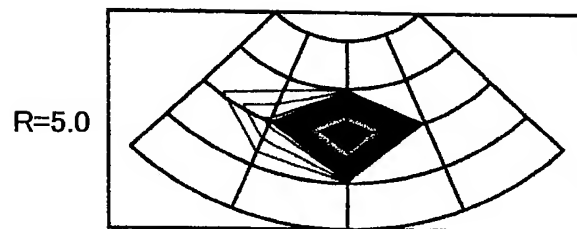


FIG.25(b)

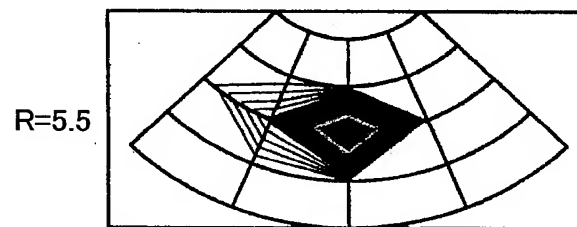


FIG.25(c)

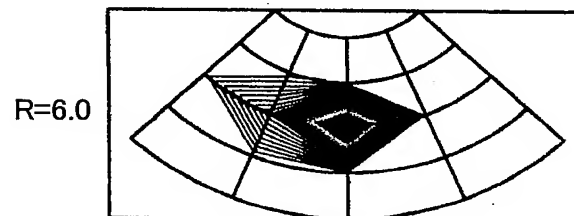


FIG.26(d)

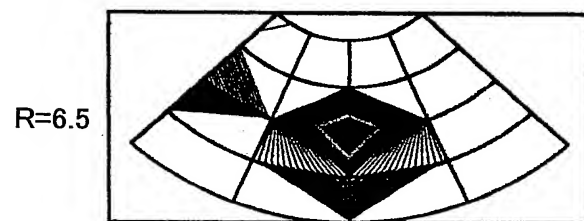


FIG.26(e)

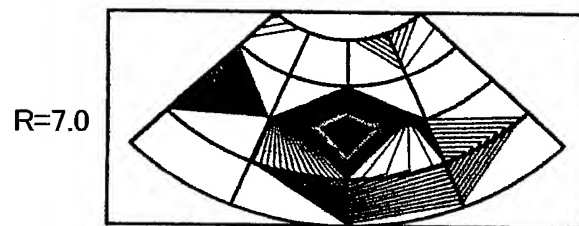


FIG.26(f)

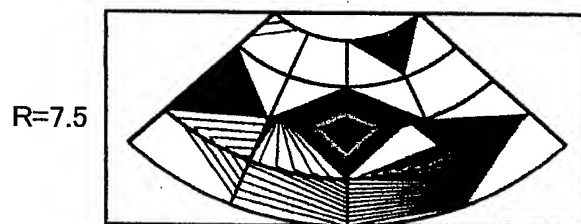
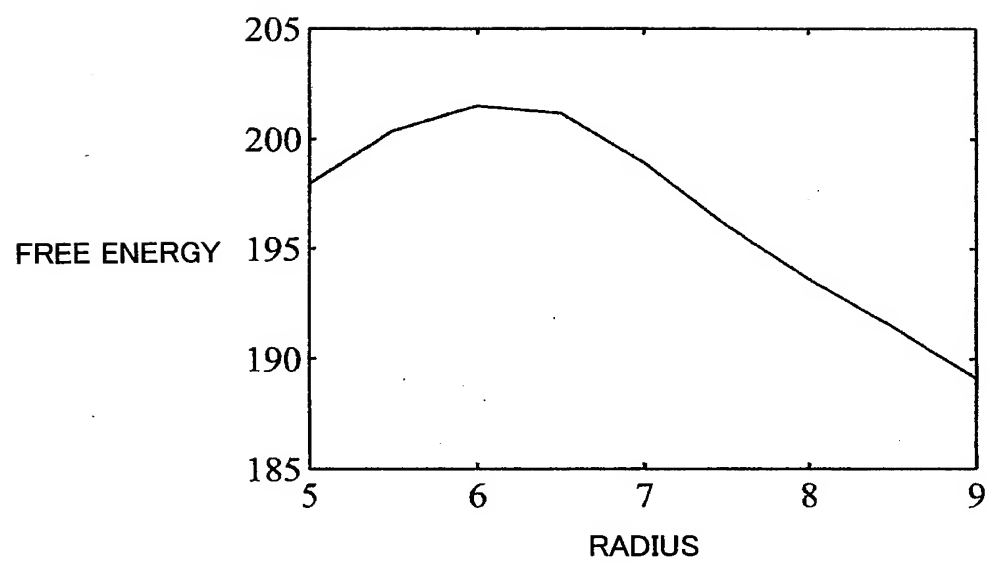




FIG.27



[Document Name] Abstract

[Abstract]

[Subject] A brain current source estimating method that enables estimation of a position or distribution, depth direction inclusive, of a brain current source from observed data is provided.

[Solving Means] Based on the fact that by causing an appropriate current flow on a virtual curved surface between a current source and an observation surface, an electromagnetic field generated by the current source can be recovered, and that as the curved surface comes closer to the true current source, expansion of current distribution on the curved surface becomes smaller, Bayesian estimation of the current source that recovers the observed data is performed. In this estimation, the fact that the model posterior probability attains the maximum when the curved surface includes the current source is utilized, that is, the model posterior probability is considered, to estimate the position of the current source including the depth direction.

[Selected Drawing] Fig. 3